



# **Positron Emission Tomography**

**CERN Accelerator School**

**Small Accelerators**

**Zeegse, the Netherlands**

**A.M.J. Paans**

**Nuclear Medicine & Molecular Imaging**

**UMC Groningen**



## Elements of Life

## PET-nuclide

**Hydrogen**

**$^{18}\text{F}$  (110 min)**

**Carbon**

**$^{11}\text{C}$  (20 min)**

**Nitrogen**

**$^{13}\text{N}$  (10 min)**

**Oxygen**

**$^{15}\text{O}$  (2 min)**



10	Ne 20,1797	Ne 16	Ne 17 109,2 ms $\beta^+$ 8,0; 13,5... $\beta\beta$ 4,59; 3,77; 5,12...; $\beta\alpha$ $\gamma$ 495; 6129*...	Ne 18 1,67 s $\beta^+$ 3,4... $\gamma$ 1042...	Ne 19 17,22 s $\beta^+$ 2,2... $\gamma$ (110; 197; 1357)	Ne 20 90,48	Ne 21 0,27	Ne 22 9,25	Ne 23 37,2 s $\beta^-$ 4,4... $\gamma$ 440; 1639...	Ne 24 3,38 m $\beta^-$ 2,0... $\gamma$ 874	Ne 25 602 ms $\beta^-$ 7,3... $\gamma$ 90; 980...	Ne 26 197 ms $\beta^-$ $\gamma$ 83; 233...	Ne 27 32 ms $\beta^-$ $\beta n$	
	F 18,998403	F 15	F 16	F 17 64,8 s $\beta^+$ 1,7 no $\gamma$	F 18 109,7 m $\beta^+$ 0,6 no $\gamma$	F 19 100	F 20 11,0 s $\beta^-$ 5,4... $\gamma$ 1634...	F 21 4,16 s $\beta^-$ 5,3; 5,7... $\gamma$ 351; 1395...	F 22 4,23 s $\beta^-$ 5,5... $\gamma$ 1275; 2083; 2166...	F 23 2,23 s $\beta^-$ 8,5... $\gamma$ 1701; 2129; 1822; 3431...	F 24 0,34 s $\beta^-$ $\gamma$ 1982	F 25 59 ms $\beta^-$ $\beta n$	F 26	
9	O 12	O 13 8,58 ms $\beta^+$ 16,7... $\beta\beta$ 1,44; 6,44... $\gamma$ (4439*; 3500...)	O 14 70,59 s $\beta^+$ 1,8; 4,1... $\gamma$ 2313...	O 15 2,03 m $\beta^+$ 1,7 no $\gamma$	O 16 99,762 $\sigma_{n,\alpha}$ 0,24	O 17 0,038 $\sigma_{n,\alpha}$ 0,24	O 18 0,200 $\sigma_{n,\alpha}$ 0,00016	O 19 27,1 s $\beta^-$ 3,3; 4,7... $\gamma$ 197; 1357...	O 20 13,5 s $\beta^-$ 2,8... $\gamma$ 1057...	O 21 3,4 s $\beta^-$ 6,4... $\gamma$ 1730; 3517; 280; 1787...	O 22 2,25 s $\beta^-$ $\gamma$ 72; 637; 1862...	O 23 82 ms $\beta^-$ $\beta n$	O 24 61 ms $\beta^-$ $\beta n$	
	N 11	N 12 11,0 ms $\beta^+$ 16,4... $\gamma$ 4439... $\beta\alpha$ 0,2...	N 13 9,96 m $\beta^+$ 1,2 no $\gamma$	N 14 99,634 $\sigma_{n,p}$ 1,8	N 15 0,366 $\sigma_{n,\alpha}$ 0,00004	N 16 7,13 s $\beta^-$ 4,3; 10,4... $\gamma$ 6329; 7115 $\beta\alpha$ 1,76...	N 17 4,17 s $\beta^-$ 3,2; 8,7... $\beta n$ 1,17; 0,38... $\gamma$ 871; 2184; $\beta\alpha$ 1,25; 1,41	N 18 0,63 s $\beta^-$ 8,4; 11,9... $\gamma$ 1982; 822; 1652; 2473... $\beta\alpha$ 1,08; 1,41... $\beta n$ 1,35; 2,46...	N 19 329 ms $\beta^-$ $\beta n$ $\gamma$ 96; 3138; 709	N 20 142 ms $\beta^-$	N 21 95 ms $\beta^-$	N 22 24 ms $\beta^-$ $\beta n$	N 23	
C 9 126,5 ms $\beta^+$ 15,5... $\beta\beta$ 8,24; 10,92... $\beta\alpha$	C 10 19,3 s $\beta^+$ 1,9... $\gamma$ 718; 1022	C 11 20,36 m $\beta^+$ 1,0 no $\gamma$	C 12 98,90 $\sigma_{n,\alpha}$ 0,0035	C 13 1,10 $\sigma_{n,\alpha}$ 0,0014	C 14 5730 a $\beta^-$ 0,2 no $\gamma$	C 15 2,45 s $\beta^-$ 4,5; 9,8... $\gamma$ 5298...	C 16 0,747 s $\beta^-$ 4,7; 7,9... $\beta n$ 0,79; 1,72	C 17 193 ms $\beta^-$ $\beta n$ 1,62... $\gamma$ 1375; 1849; 2499...	C 18 92 ms $\beta^-$ $\gamma$ 2614; 880; 2499... $\beta n$ 0,88; 1,55...	C 19 49 ms $\beta^-$ $\beta n$ 1,01; 0,46...	C 20 14 ms $\beta^-$ $\beta n$		C 22	
B 8 770 ms $\beta^+$ 14,1... $2\alpha$ - 1,6; 8,3	B 9	B 10 19,9 $\sigma_{n,\alpha}$ 0,5 $\sigma_{n,\alpha}$ 3840	B 11 80,1 $\sigma_{n,\alpha}$ 0,005	B 12 20,20 ms $\beta^-$ 13,4... $\gamma$ 4439... $\beta\alpha$ 0,2...	B 13 17,33 ms $\beta^-$ 13,4... $\gamma$ 3684 $\beta n$ 3,6; 2,4...	B 14 13,8 ms $\beta^-$ 14,0... $\gamma$ 6090; 6730 $\beta n$	B 15 10,4 ms $\beta^-$ $\beta n$ 1,77; 3,20...	B 17 5,1 ms $\beta^-$ $\beta n$ ; $\beta 2n$ ; $\beta 3n$ ; $\beta 4n$						
Be 7 53,29 d 478 $n, p$ 39000	Be 8	Be 9 100 $\sigma_{n,\alpha}$ 0,008	Be 10 $1,6 \cdot 10^6$ a $\beta^-$ 0,6 no $\gamma$	Be 11 13,8 s $\beta^-$ 11,5... $\gamma$ 2125; 6791... $\beta\alpha$ 0,77...	Be 12 23,6 ms $\beta^-$ 11,7... $\beta n$	Be 14 4,35 ms $\beta^-$ $\beta n$ < 0,8; 3,02; 3,52...; $\beta 2n$ $\gamma$ 3528*; 3680*								
Li 6 7,5 $\sigma_{n,\alpha}$ 0,039 $n, \alpha$ 940	Li 7 92,5 $\sigma_{n,\alpha}$ 0,045	Li 8 840,3 ms $\beta^-$ 12,5 $\beta 2\alpha$ ~ 1,6	Li 9 178,3 ms $\beta^-$ 13,6... $\beta n$ 0,7... $\beta\alpha$	Li 10	Li 11 8,5 ms $\beta^-$ ~ 18,5; 20,4 $\gamma$ 3368*; 320... $\beta n$ $\beta 2n$ ; $\beta 3n$ ; $\beta\alpha$ ; $\beta 1$									

16

12

14

10



**PET:**

**A multidisciplinary approach**

**Cyclotron  
Chemistry**

**radionuclides, simple form  
on-line/off-line synthesis  
labeled compound  
purification**

**Pharmacy  
Medicine**

**pharmaceutical quality, QC  
PET-scan  
evaluation, compartment model**

**A joint effort/multidisciplinary approach**

**Chemistry  
Medicine  
Pharmacy  
Physics**



# SCX-MC17



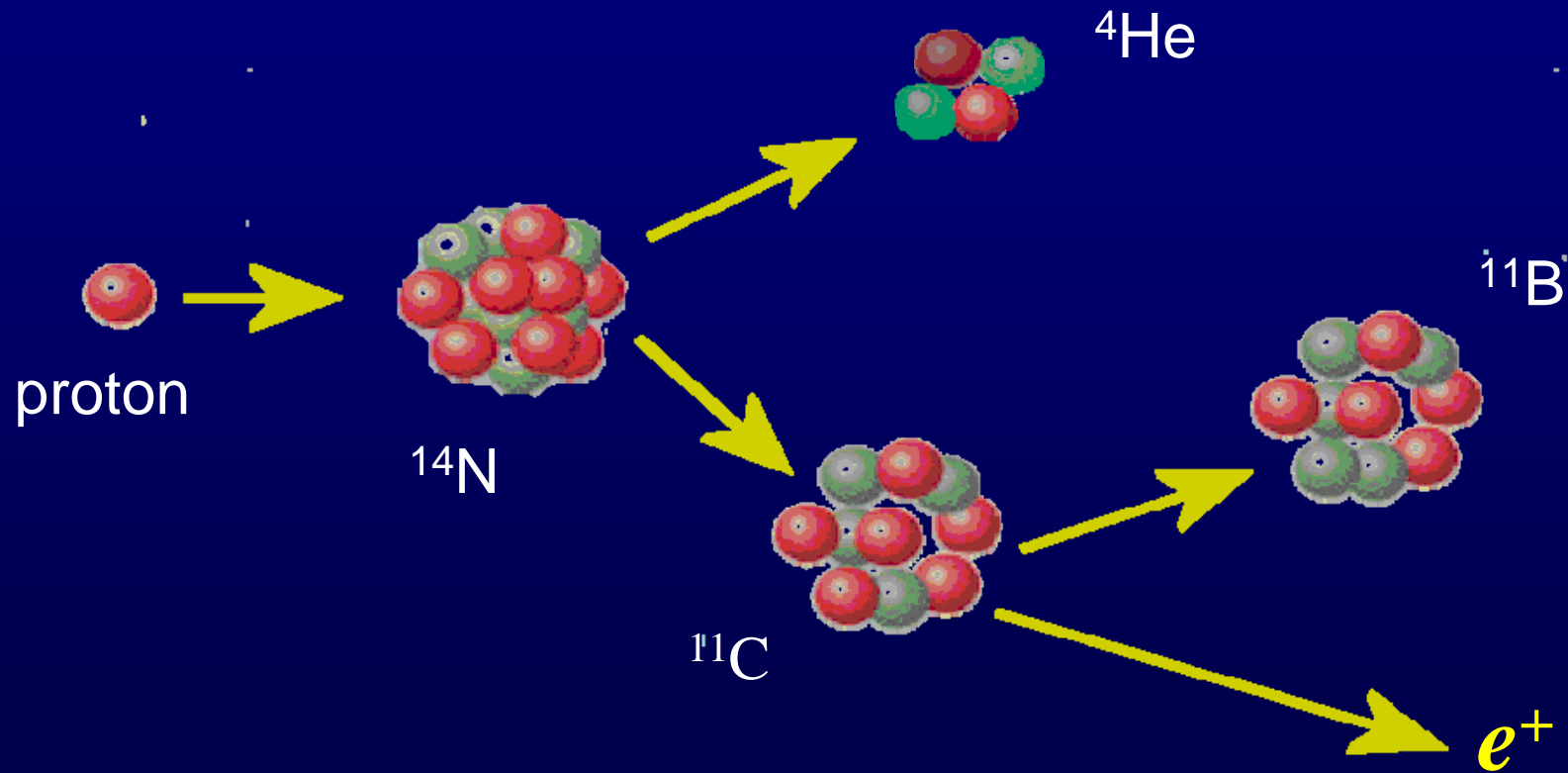


Nuclear Reaction	Q-value	Target	Product
$^{18}\text{O}(p,n)^{18}\text{F}$	- 2.4 MeV	$\text{H}_2^{18}\text{O}$ $^{18}\text{O}_2 (+\text{F}_2)$	$^{18}\text{F}^-$ $^{18}\text{F}_2$
$^{20}\text{Ne}(d,\alpha)^{18}\text{F}$	+ 2.8 MeV	$\text{Ne} (+\text{F}_2)$	$^{18}\text{F}_2$
$^{14}\text{N}(p,\alpha)^{11}\text{C}$	- 2.9 MeV	$\text{N}_2 (+\text{O}_2)$	$^{11}\text{CO}_2$
$^{16}\text{O}(p,\alpha)^{13}\text{N}$	-5.2 MeV	$\text{H}_2\text{O}$ + EtOH	$^{13}\text{NO}_3, ^{13}\text{NO}_2$ $^{13}\text{NH}_3$
$^{14}\text{N}(d,n)^{15}\text{O}$	+ 5.1 MeV	$\text{N}_2 (+\text{O}_2)$	$^{15}\text{O}_2$
$^{15}\text{N}(p,n)^{15}\text{O}$	- 3.5 MeV	$^{15}\text{N}_2 (+\text{O}_2)$	$^{15}\text{O}_2$





# Positron Emitters: Production and decay





**Specific activity      Theoretical:  $A \text{ (Bq)} = N_0 \cdot \lambda$**

$$^{11}\text{C} \quad 9.2 \times 10^9 \text{ Ci/mol} \quad = \quad 340 \text{ TBq}/\mu\text{mol}$$

$$^{13}\text{N} \quad 1.9 \times 10^{10} \text{ Ci/mol} \quad = \quad 700 \text{ TBq}/\mu\text{mol}$$

$$^{15}\text{O} \quad 9.2 \times 10^{10} \text{ Ci/mol} \quad = \quad 3400 \text{ TPBq}/\mu\text{mol}$$

$$^{18}\text{F} \quad 1.7 \times 10^9 \text{ Ci/mol} \quad = \quad 63 \text{ TBq}/\mu\text{mol}$$

**For comparison**

$$^{14}\text{C} \quad 6.2 \times 10^1 \text{ Ci/mol} \quad = \quad 2.3 \text{ MBq}/\text{mmol}$$



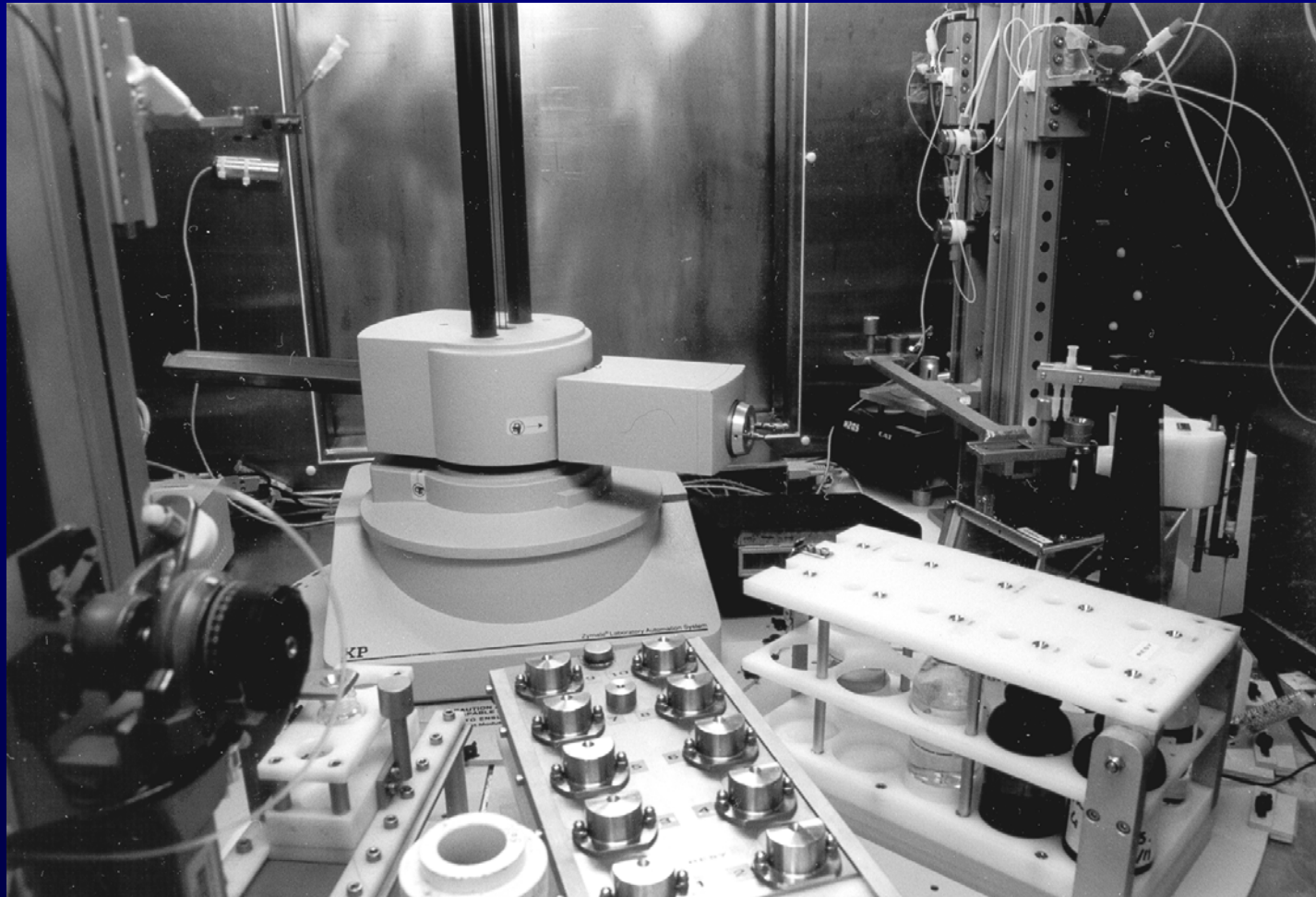


## “Hot cells” in the radiochemistry lab



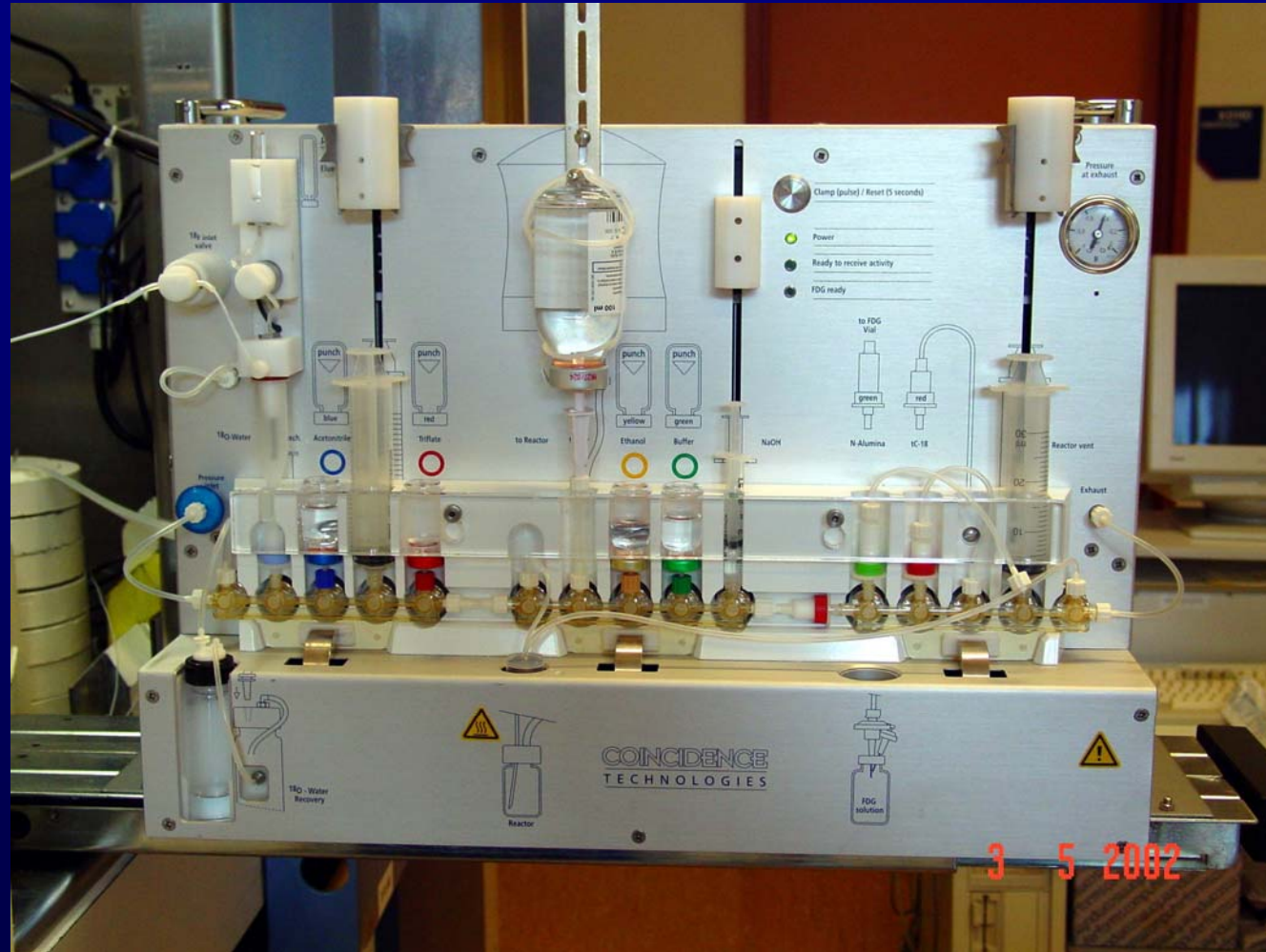


# Radiochemistry with robotics





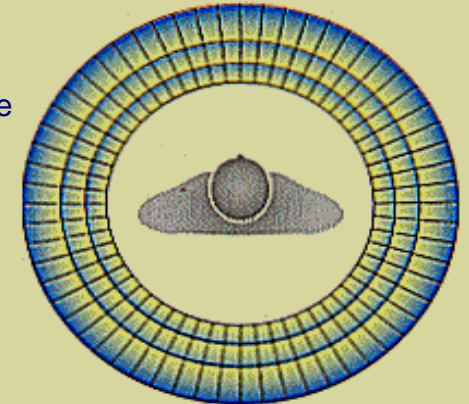
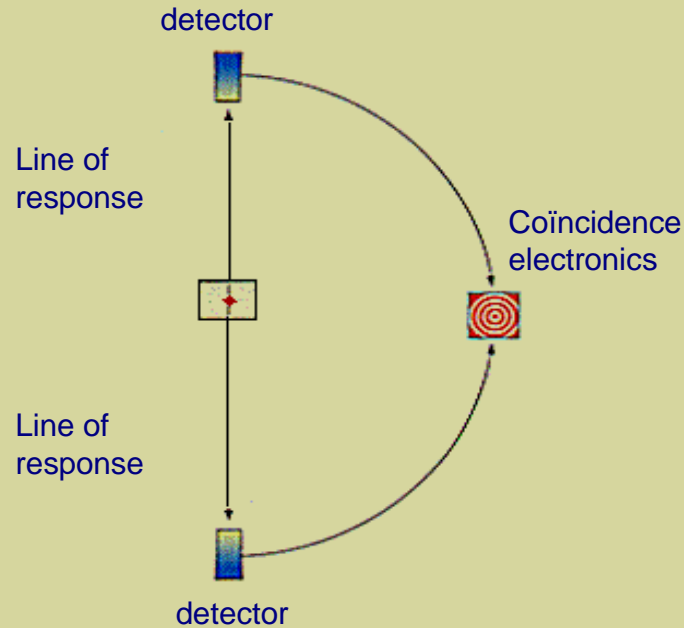
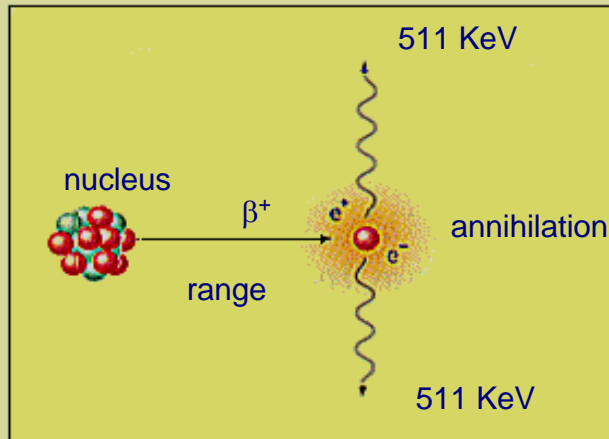
# FDG-module ready for synthesis







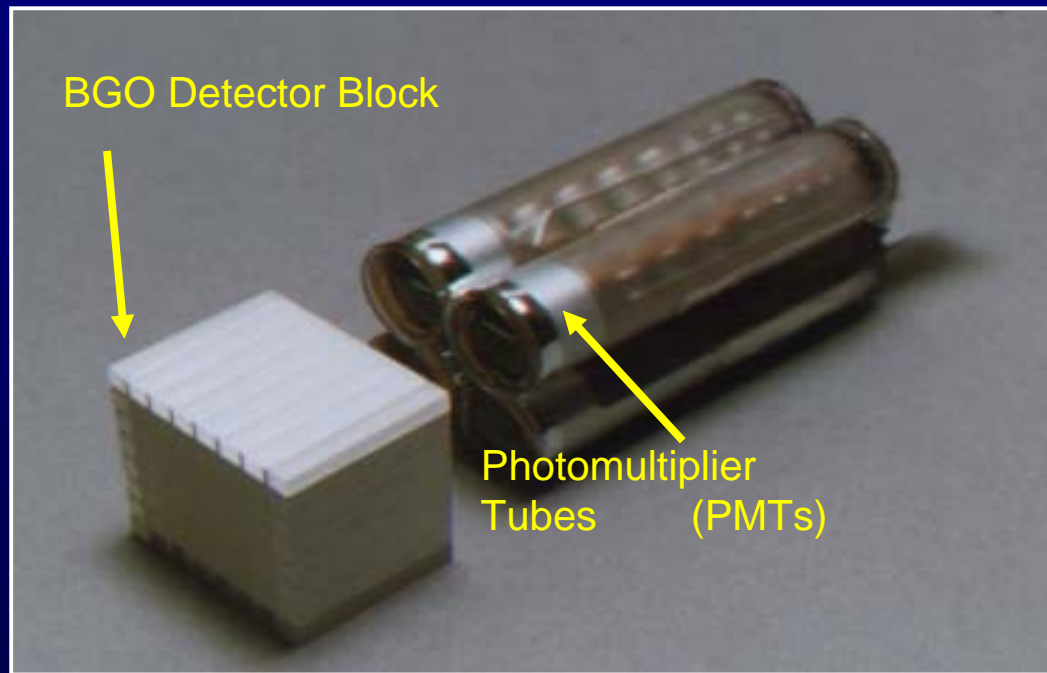
# Annihilation & coincidence detection



Detector rings



<b>Detector materials</b>	<b>NaI</b>	<b>BGO</b>	<b>GSO</b>	<b>LSO</b>
<b>Density (g/cc)</b>	<b>3.67</b>	<b>7.13</b>	<b>6.7</b>	<b>7.4</b>
<b>Eff Atomnumber</b>	<b>51</b>	<b>75</b>	<b>59</b>	<b>66</b>
<b>Hygroscopic</b>	<b>yes</b>	<b>no</b>	<b>no</b>	<b>no</b>
<b>Decay time (ns)</b>	<b>230</b>	<b>300</b>	<b>56/600</b>	<b>40</b>
<b>Rel light yield</b>	<b>100%</b>	<b>15%</b>	<b>25%</b>	<b>75%</b>
<b>Energy resolution</b>	<b>7.8%</b>	<b>10.1%</b>	<b>9.5%</b>	<b>10.%</b>



8 x 8 matrix of BGO crystals per detector

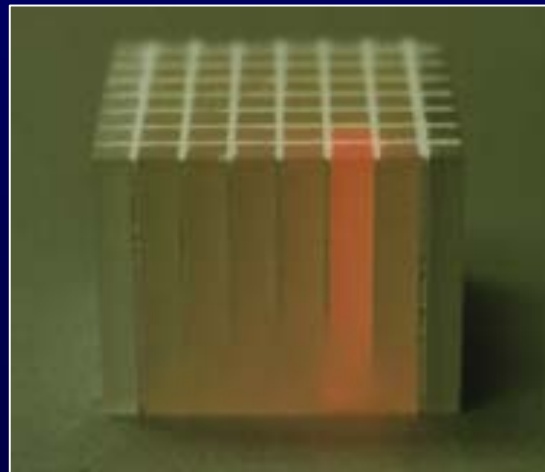
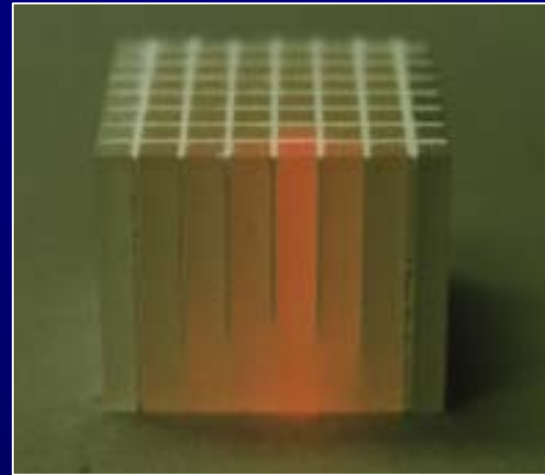
64 BGO crystal elements per detector

4 photomultiplier tubes per detector

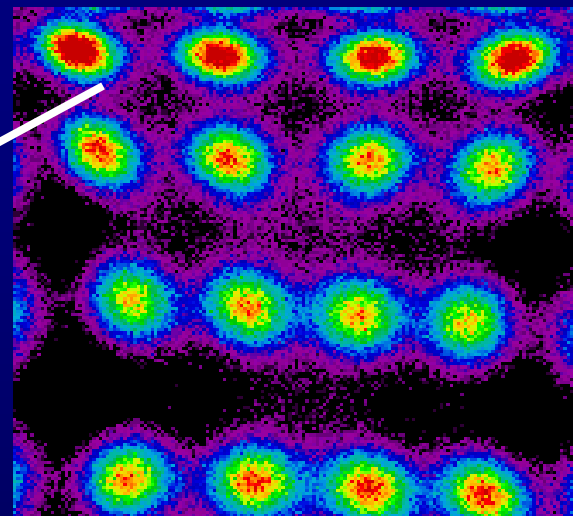
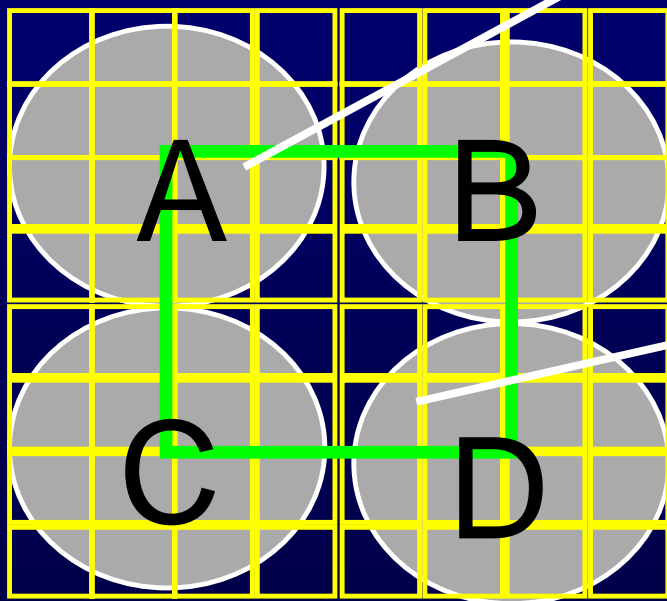


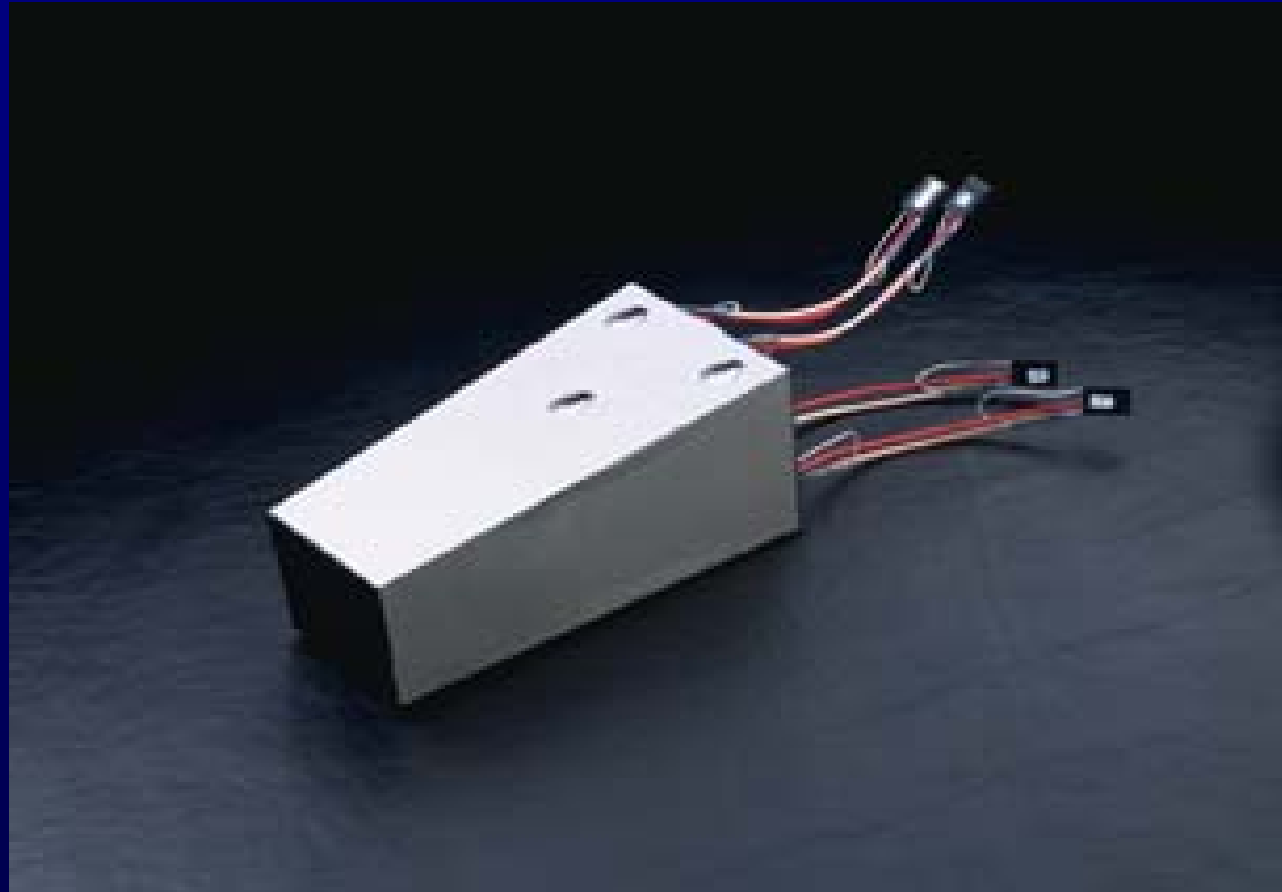


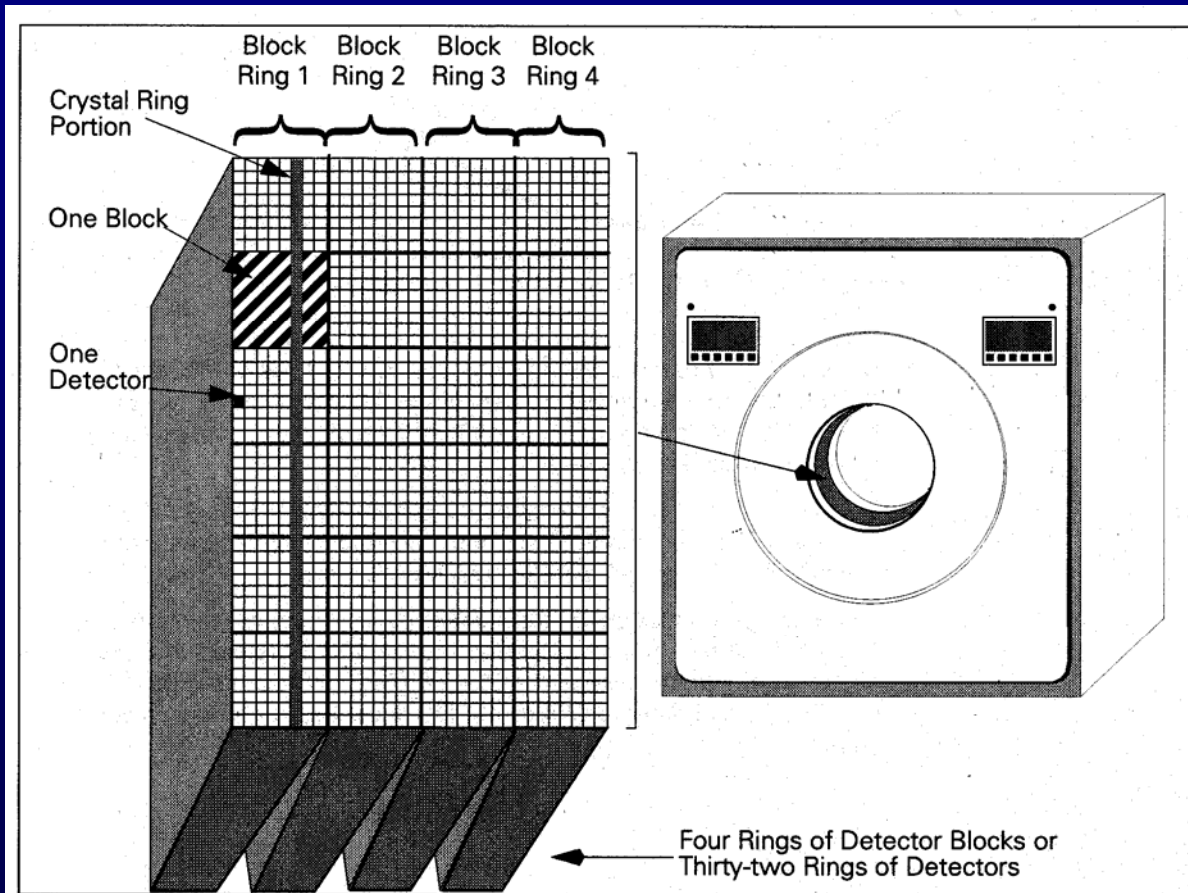
Patented light  
guides channel  
the scintillation  
light . . .



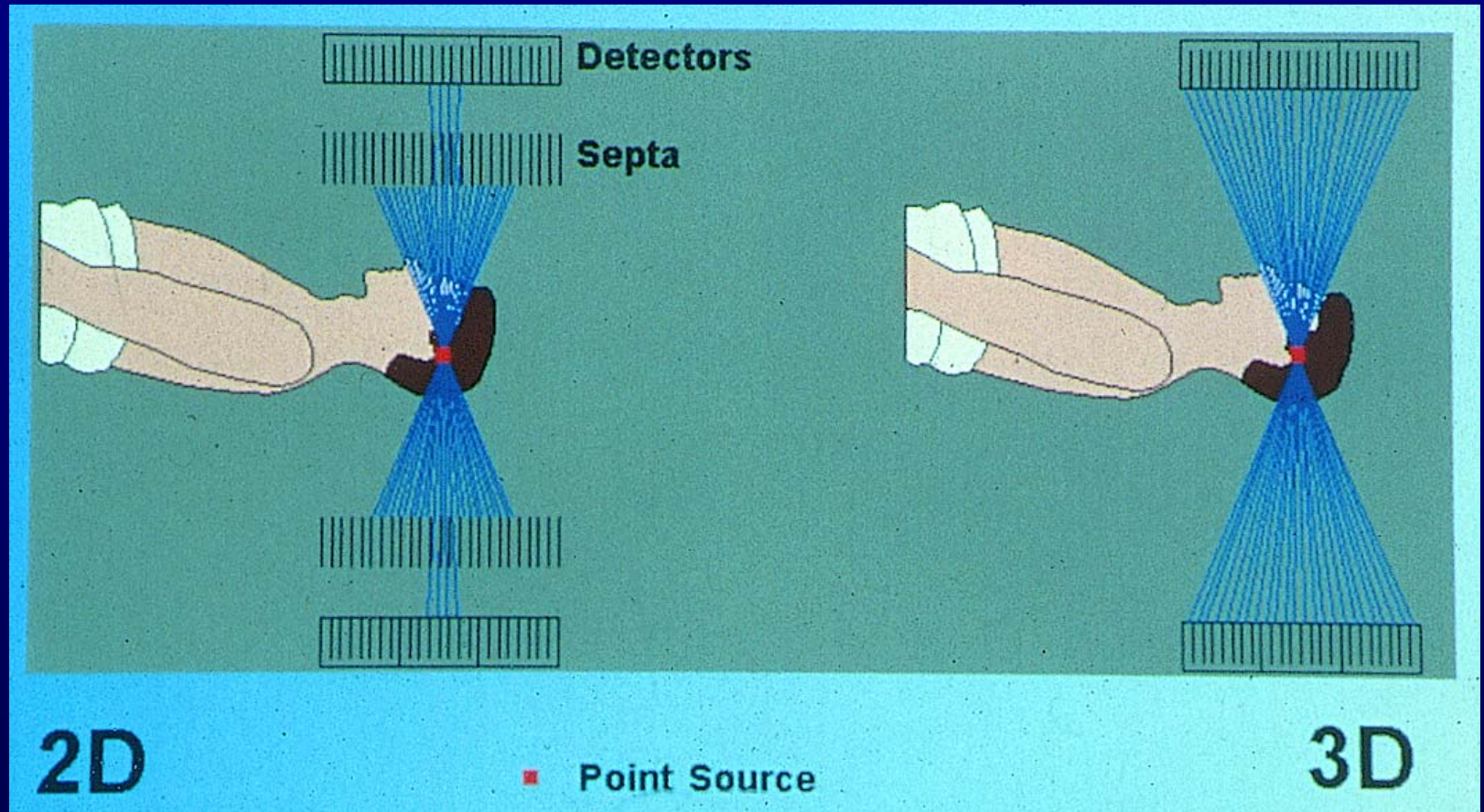
. . . producing a  
unique  
combination of  
signals in the four  
photomultiplier  
tubes (PMTs).



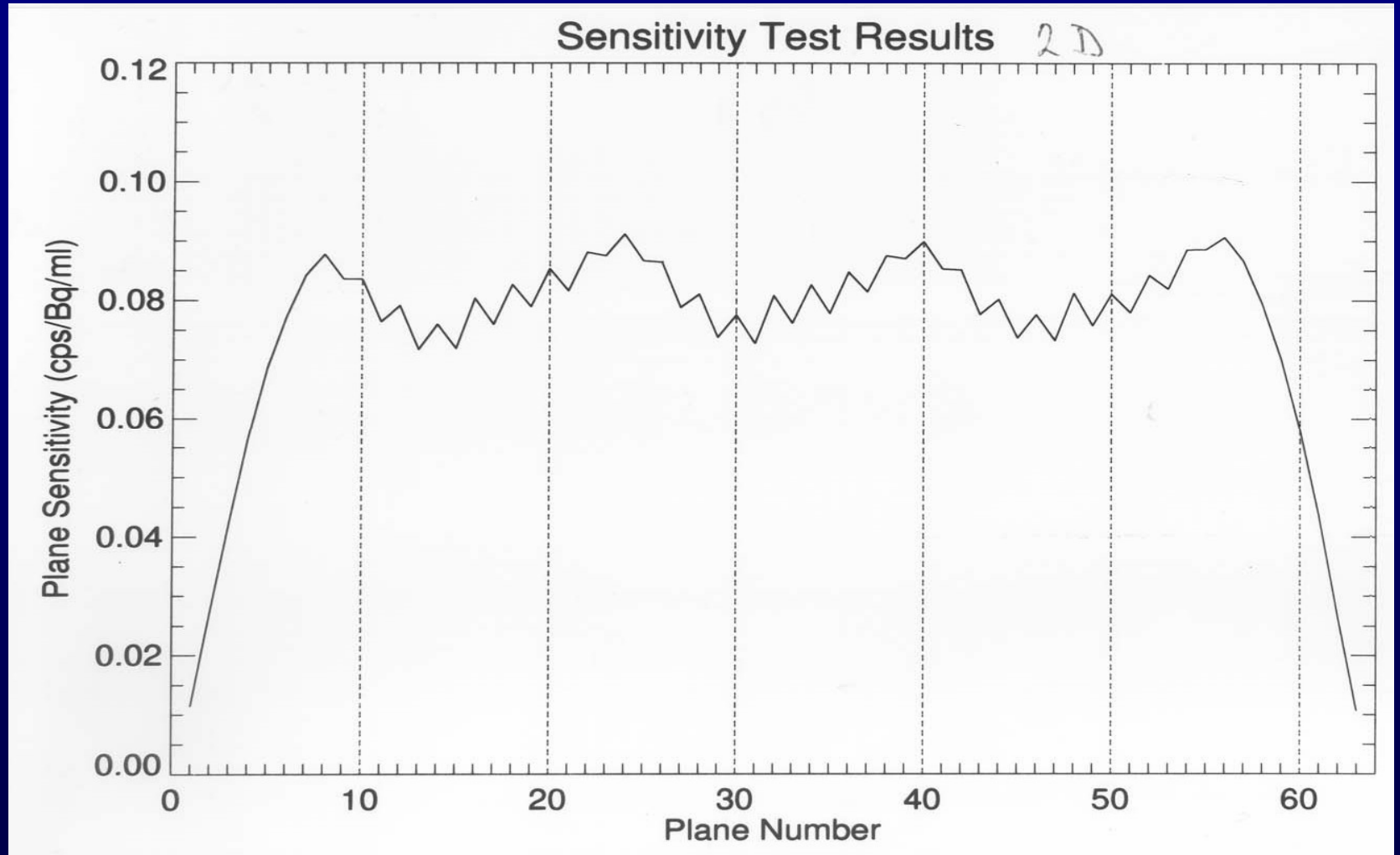




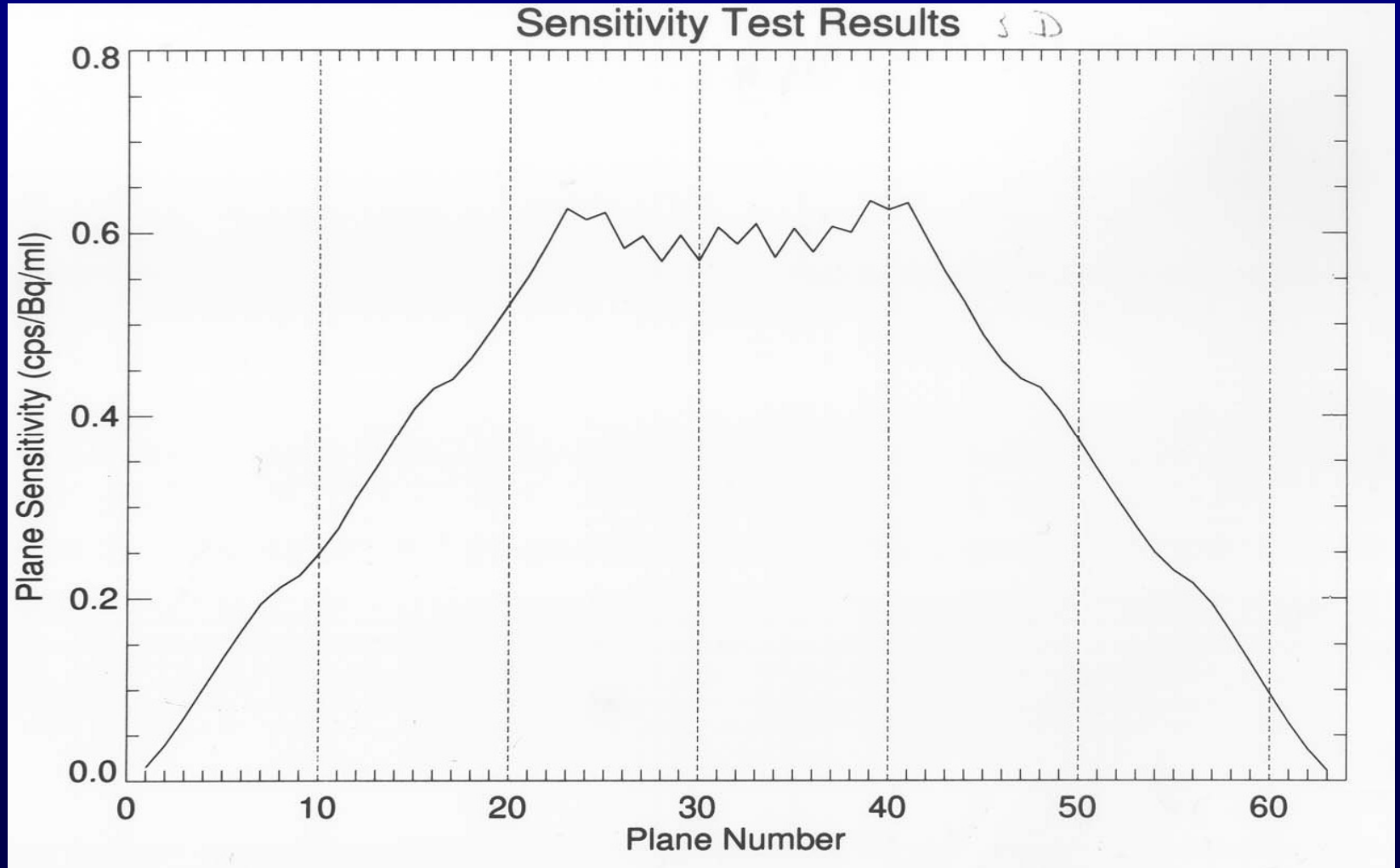
**Figure A-1.** Blocks and Detectors in an ECAT EXACT HR<sup>+</sup> Scanner.







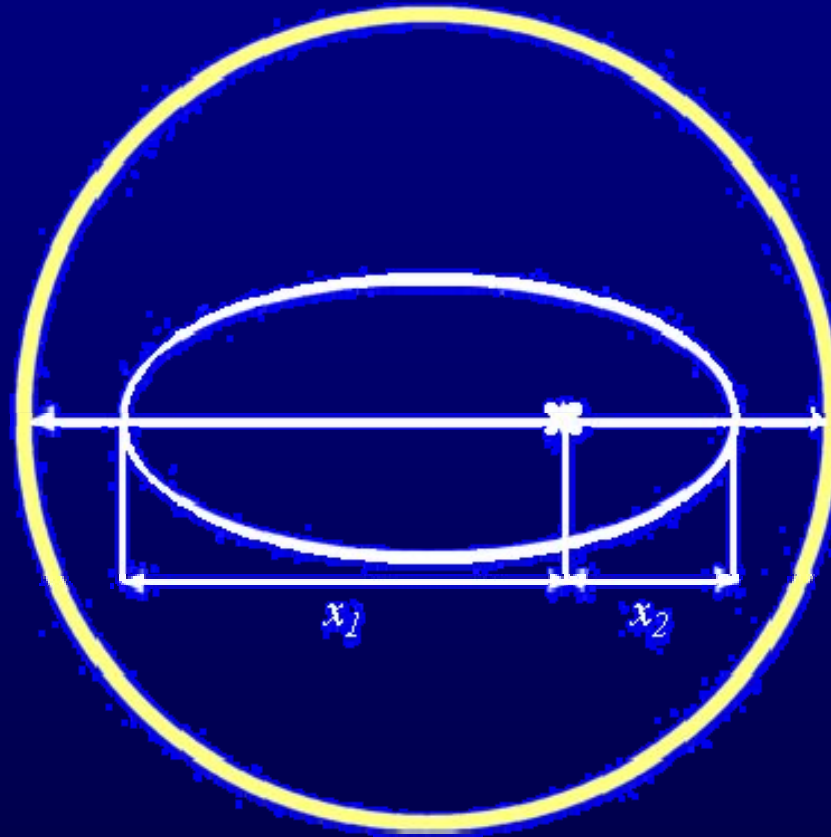








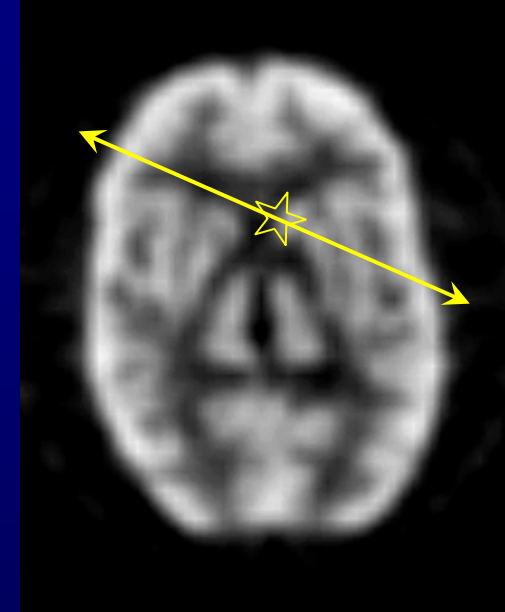
# Attenuation correction





# Attenuation correction in PET

- In coincidence detected 511 keV photons
- Attenuation is function of the effective length on the LOR
- Simple measurement with external source

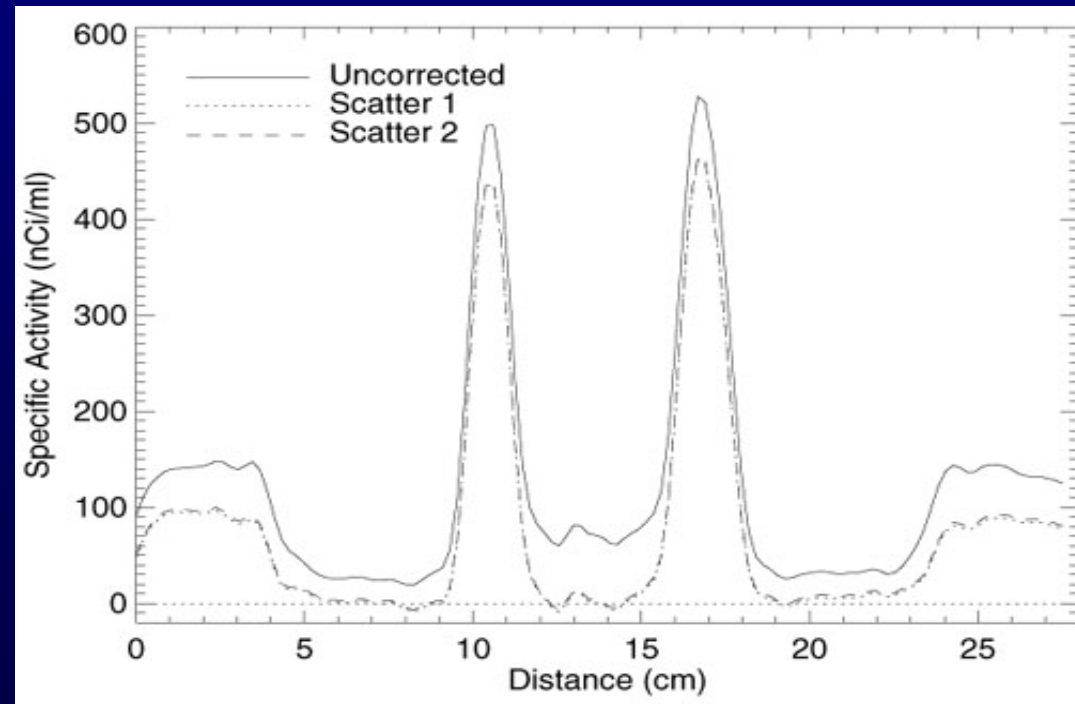
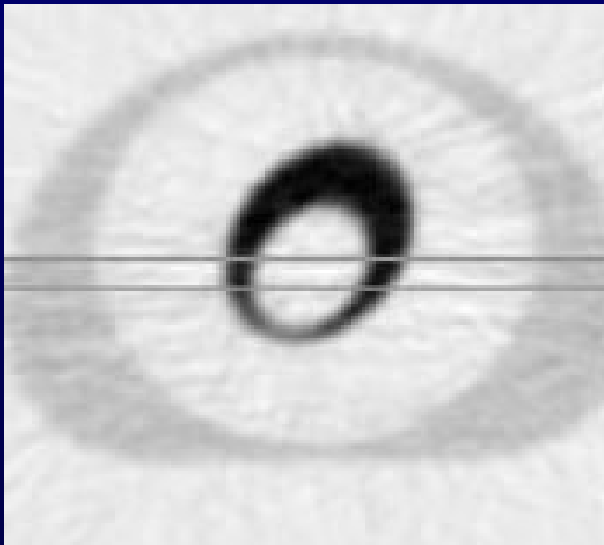


$$A_{tn} = A_{tn_1} * A_{tn_2} = e^{-\int_{x_1}^a \mu(s) ds} * e^{-\int_a^{x_2} \mu(s) ds} = e^{-\int_{x_1}^{x_2} \mu(s) ds}$$



# 3D Scatter Correction

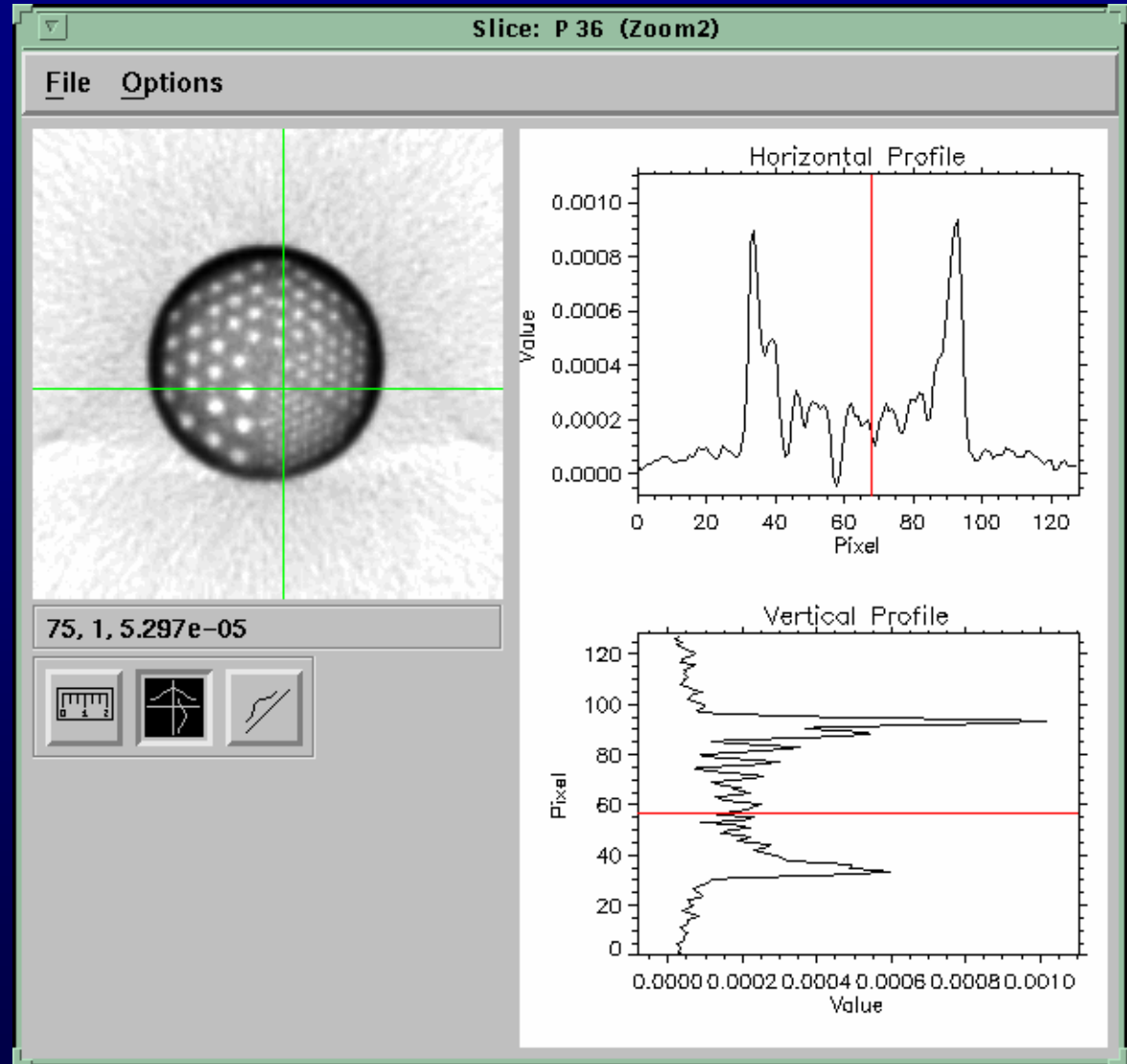
- Scatter correction based on scatter model
- Combined emission & transmission scans





# Jaszczak phantom

## NO corrections

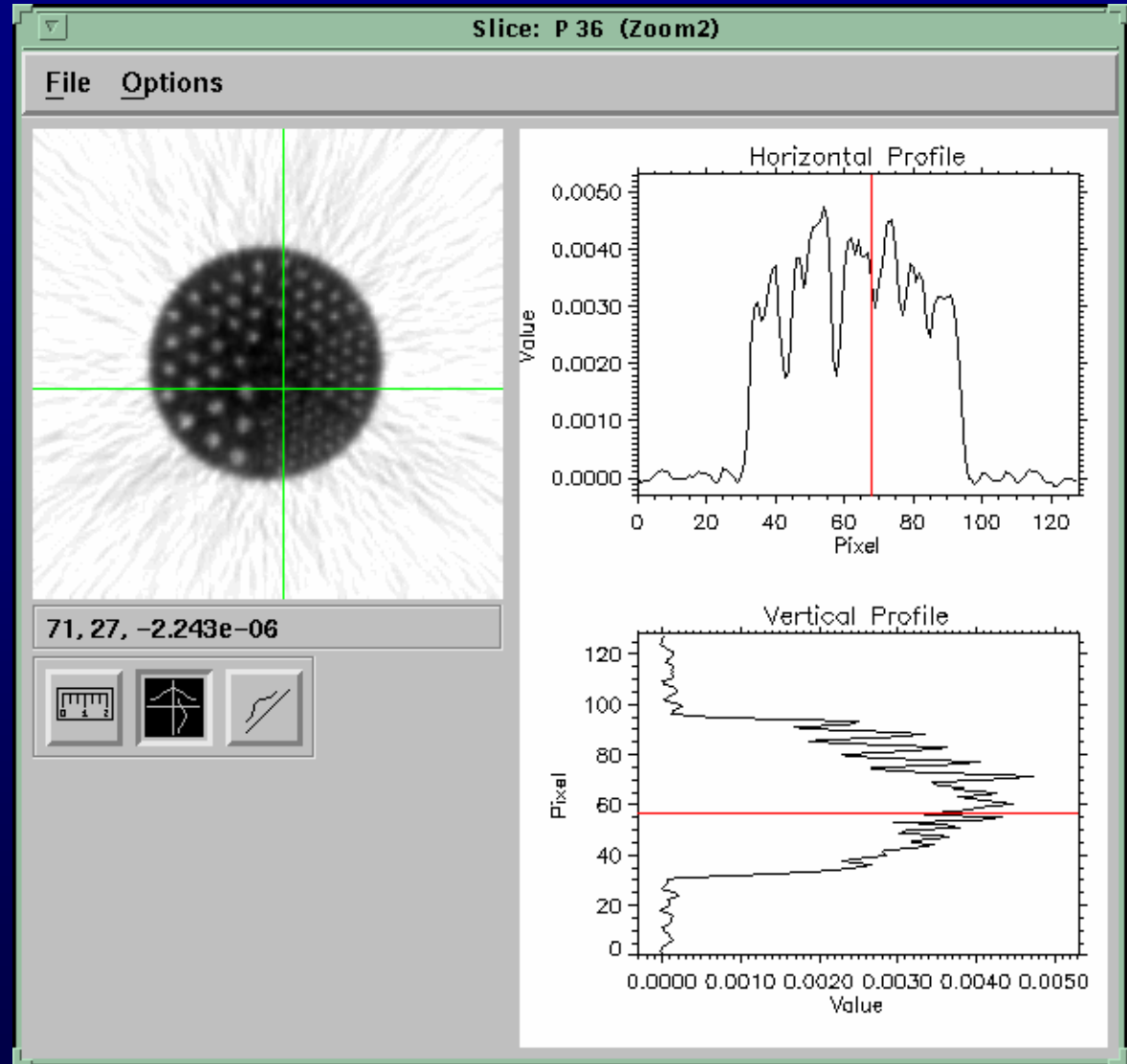






# Jaszczak phantom

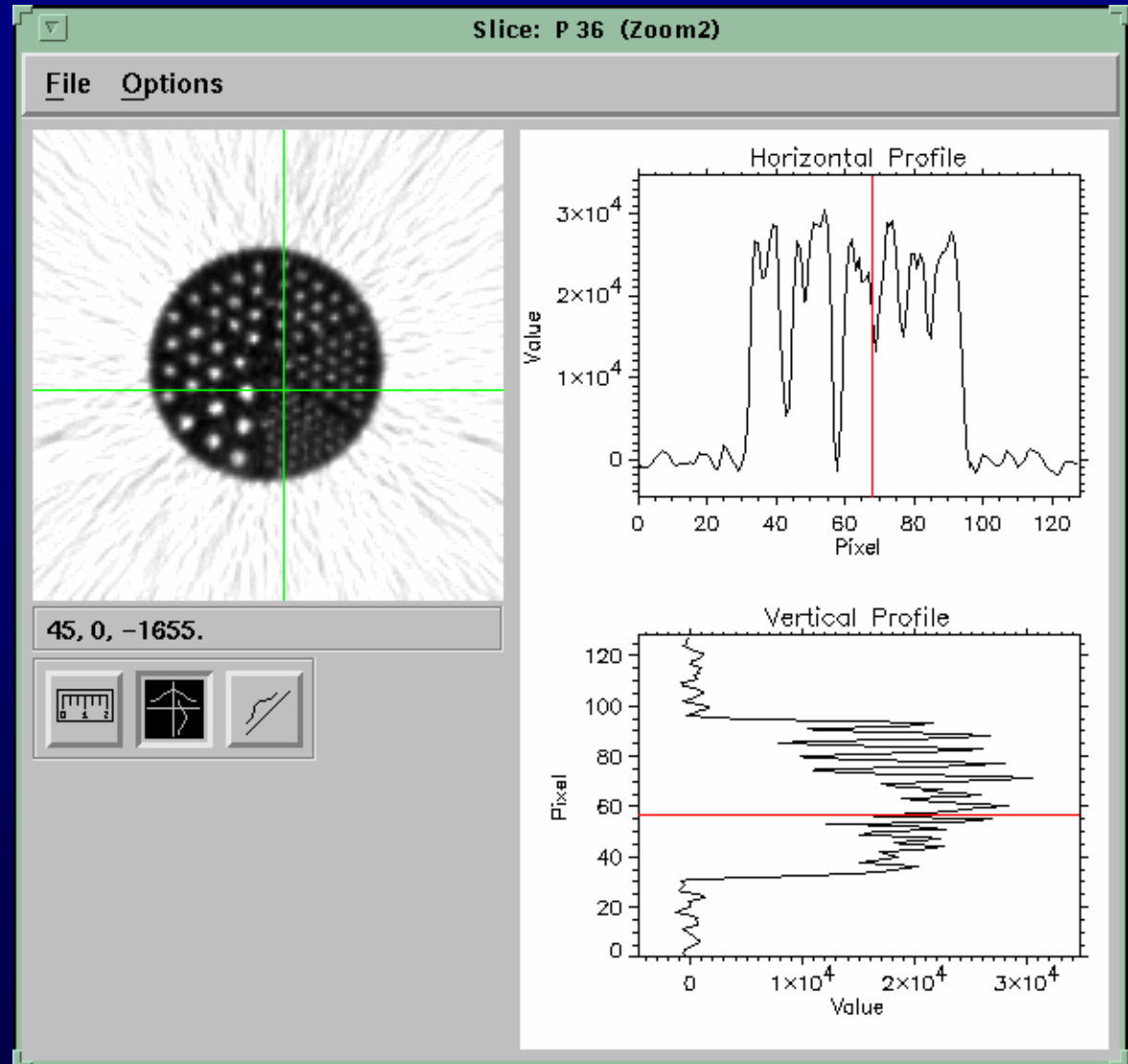
attenuation corrected





# Jaszczak phantom

attenuation & scatter corrected





## Data reconstruction

Data is generated by measuring according projection lines, line integrals

Basic reconstruction is Filtered Back Projection (FBP) according to mathematics described by Radon (1917)

Maximum Likelihood Expectation Maximization (ML-EM) is a iterative method that maximizes the probability of the reconstructed image for a given set of measured projection data.



## Data reconstruction

In PET ML-EM is successful because of Poisson statistics

Problem of iterative methods: NO objective stopping criterium and procedure will easy generate artefacts

Advantage: If stopped at the correct moment, a superior image quality with less noise

Disadvantage: the correct stopping criterium is not a general rule but has to be established per procedure



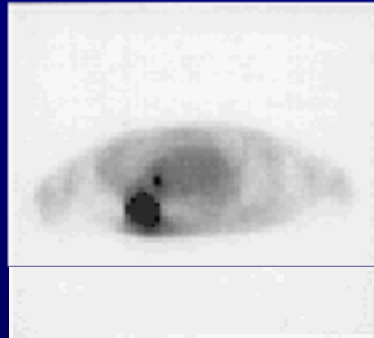
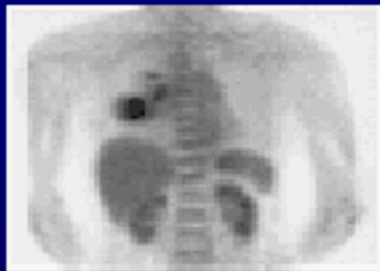
## Data reconstruction

- **FBP or ML-EM**
- **Attenuation correction**
- **Scatter correction**

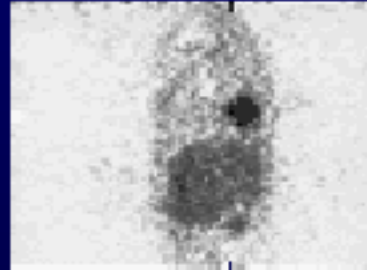
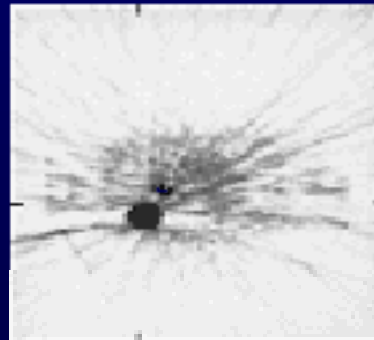


# Reconstruction Techniques

## Iterative vs Filtered Back Projection (FBP)



**Iterative  
reconstruction**



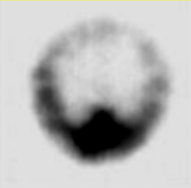




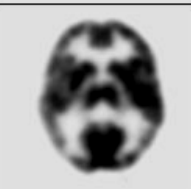
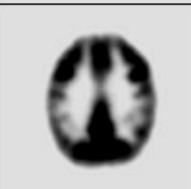

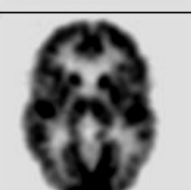
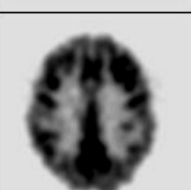
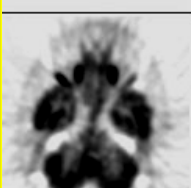
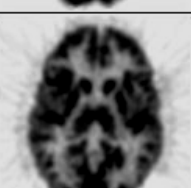
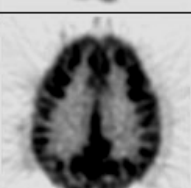


**FBP**



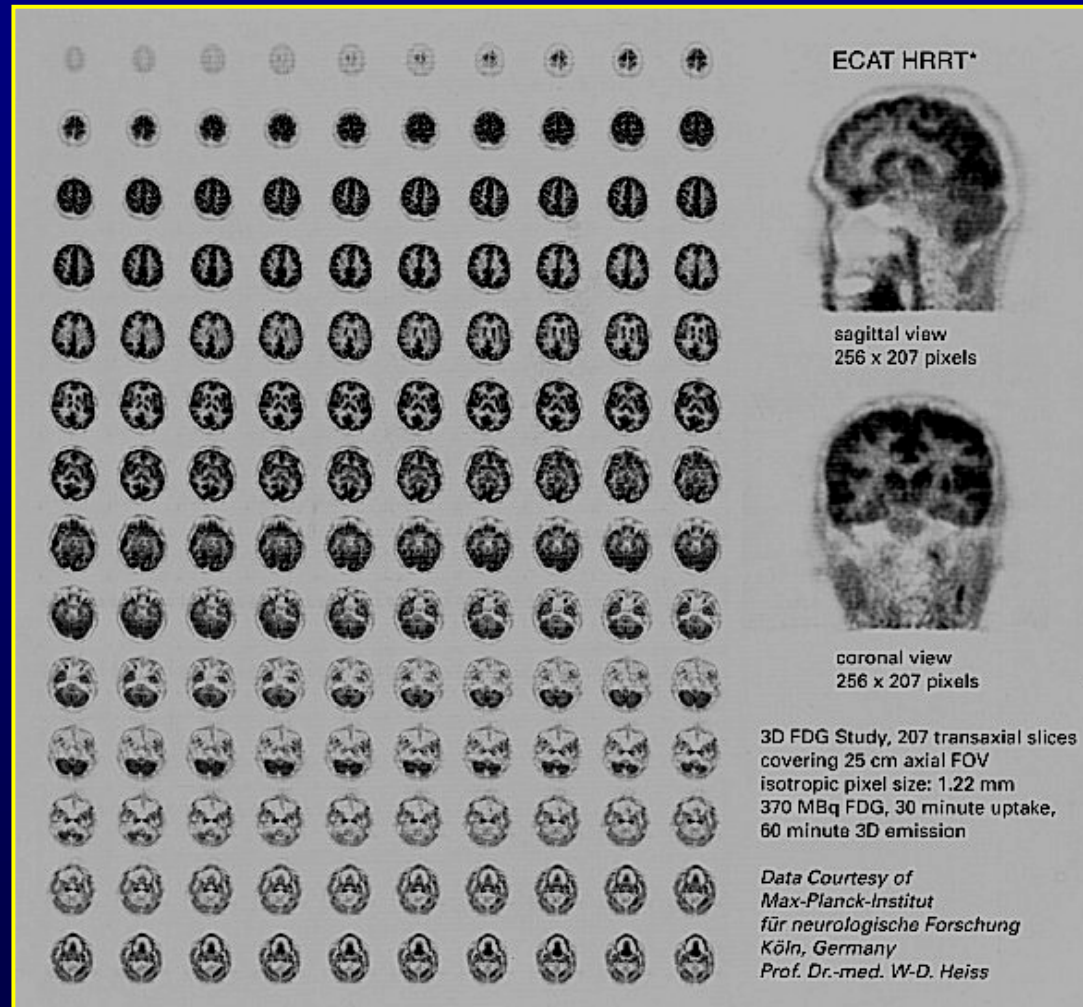


# Resolution evolution in time

			PET III 1975
			ECAT II 1977
			NeuroECAT 1978
			ECAT 931 1985
			ECAT EXACT HR+ 1995



# ECAT HRRT at MPI Cologne





## Positron energies and ranges

Nuclide	$E_{\beta\text{max}}$ (MeV)	Range (mm)	$E_{\beta\text{mean}}$ (MeV)	Range (mm)
<sup>11</sup> C	0.961	3.9	0.38	1.1
<sup>13</sup> N	1.190	5.1	0.48	1.5
<sup>15</sup> O	1.723	8.0	0.69	2.5
<sup>18</sup> F	0.635	2.3	0.25	0.6
<sup>52</sup> Fe	0.804	3.1	0.32	0.9
<sup>68</sup> Ga	1.899	8.9	0.76	2.9
<sup>75</sup> Br	1.740	8.1	0.70	2.6
<sup>82</sup> Rb	3.350	17.	1.34	5.9



## Fundamental Limitations in Spatial Resolution

### - Range of the positrons

The mean range varies from 0.6 mm ( $^{18}\text{F}$ ),  
1.1 mm ( $^{11}\text{C}$ ), 1.5 mm ( $^{13}\text{N}$ ) to 2.5 mm ( $^{15}\text{O}$ )  
or 5.9 mm ( $^{82}\text{Rb}$ )

### -Non-zero momentum at moment of annihilation

Finite angular width of  $0.5^\circ$  FWHM about the  
mean angle of  $180^\circ$



## Time Of Flight (TOF) measurement

Detectors A and B at distance  $2d$ , source at distance  $x$  from center

$$PA - PB = (d+x) - (d-x) \rightarrow dt = 2x/c$$

With  $x = 1 \text{ mm} \rightarrow dt = 3.3 \text{ ps}$

Detectors that fast and sensitive to 511 keV do not exist



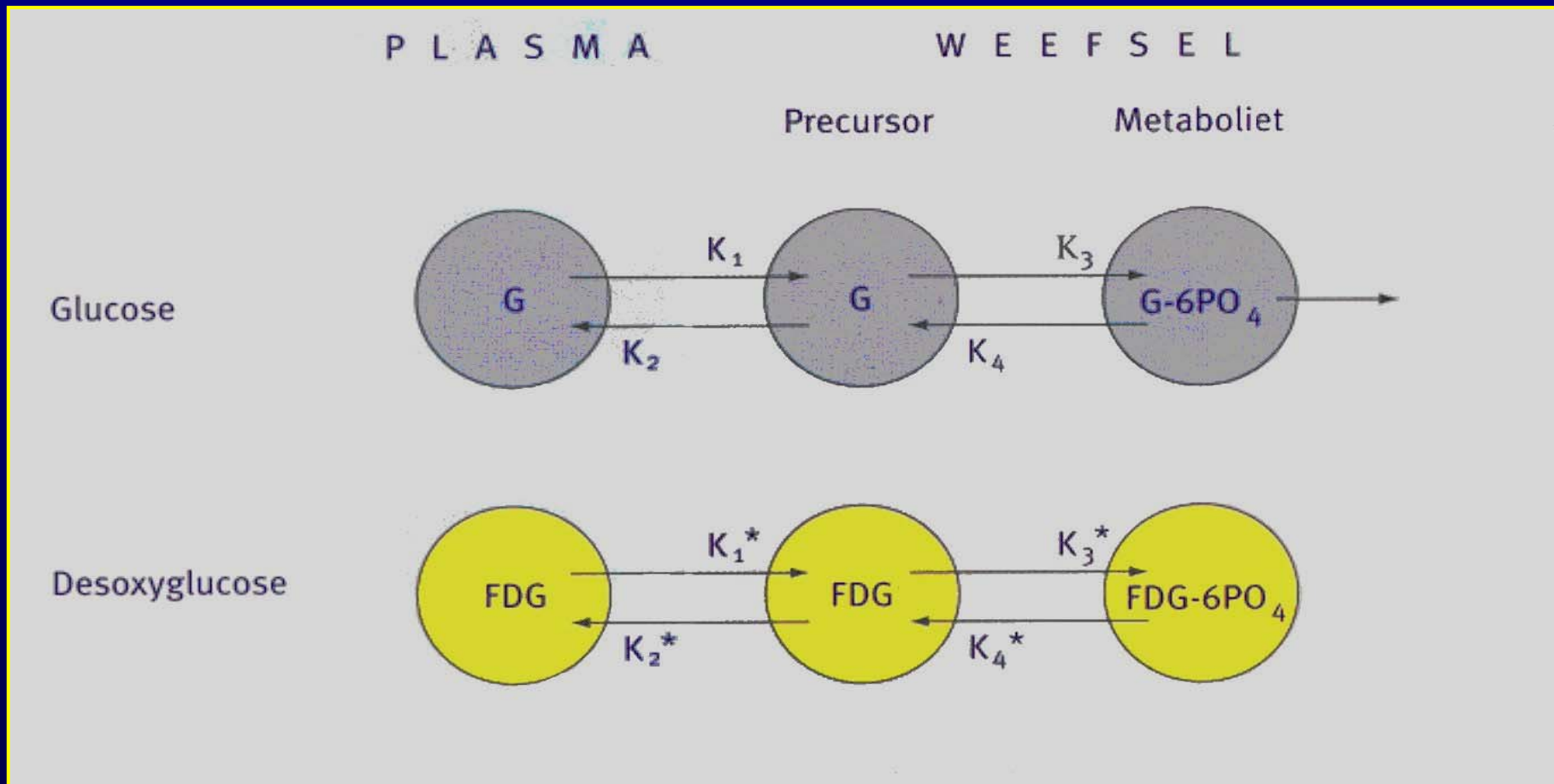
## Brain research

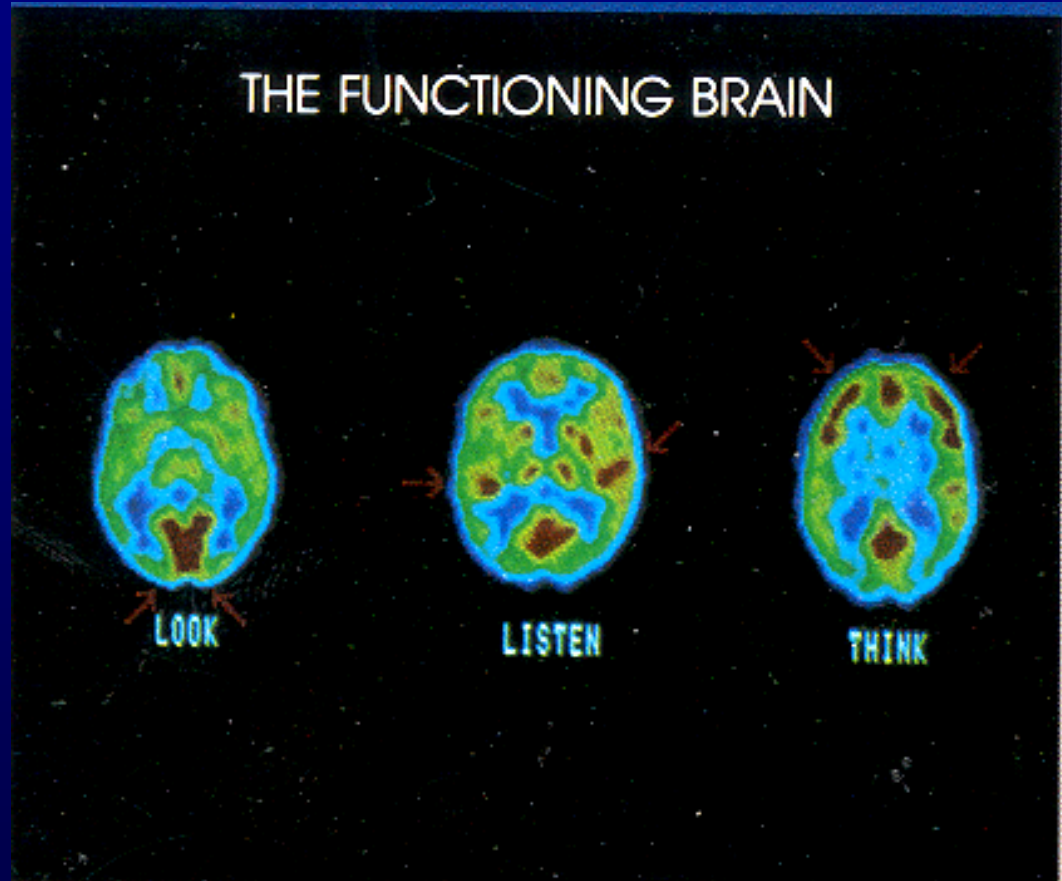
- Blood flow  $H_2^{15}O, C^{15}O_2$
  - Blood volume  $^{11}CO, C^{15}O$
  - Glucose metabolism  $^{18}FDG$
  - Tumor metabolism  $^{18}FDG, ^{11}C$ -amino acids
  - Receptor density  $^{11}C$ -raclopride,  $^{18}F$ -DOPA,  $^{18}F$ ESP
  - Stimulus research  $H_2^{15}O, ^{18}FDG$
- }oxygen extraction

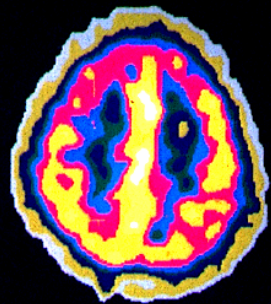




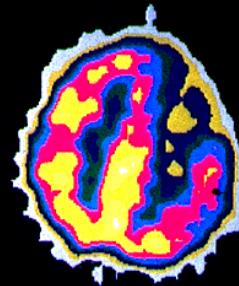
# Pathophysiology: FDG-model



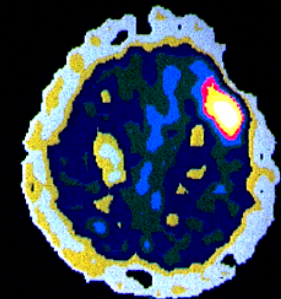




H2-15O

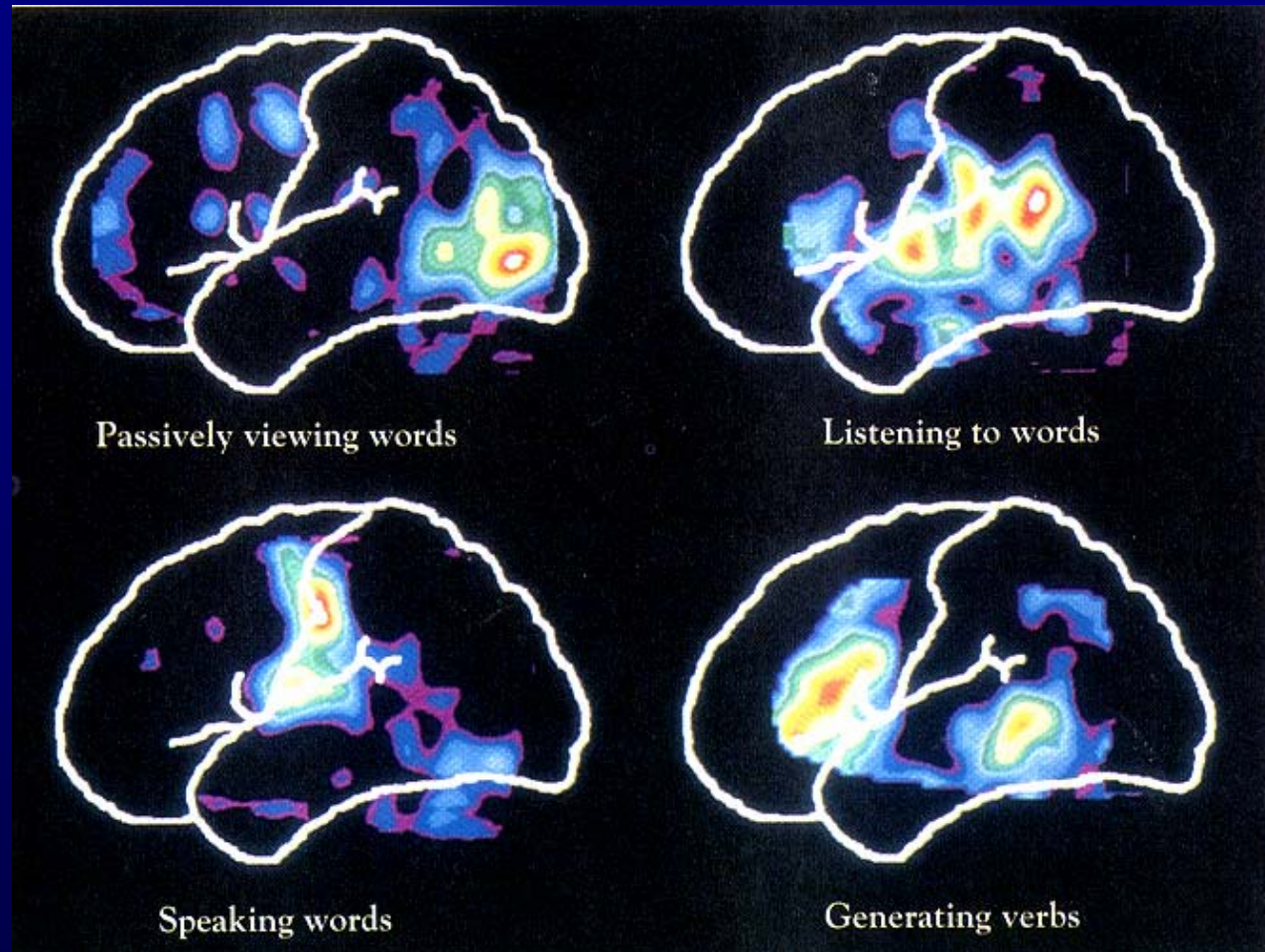


FDG



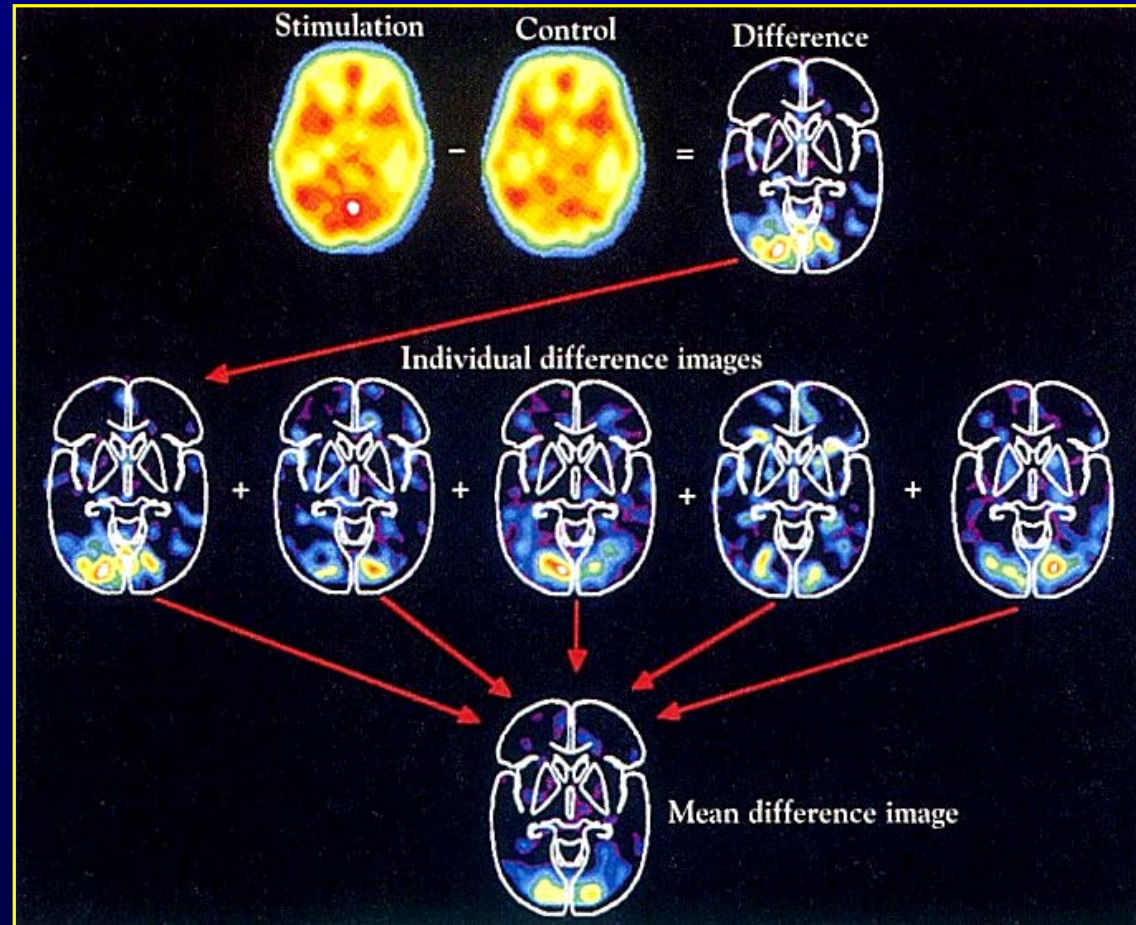
L-[1-C-11]-tyrosine







# Functional Neuro-anatomy: The Concept





# Visual stimulation vs rest

The screenshot displays the Neuro Tool interface with two side-by-side windows, each showing 'Study 1'. Each window contains three brain scan views: Transaxial (top left), Sagittal (top right), and Coronal (bottom center). The scans are color-coded, with a color bar on the right labeled 'ColorTool' showing a scale from 0% (dark blue) to 100% (red). The interface includes a menu bar with options like 'Edit Label', 'Annotate', 'Magnifier', 'View Slices', and 'Options'. A terminal window at the bottom shows a command prompt with an error message: 'petsun2[ecat]1: filler:ERROR...File vmunix.spt : No such file or directory'.





## **Language Study: Functional Brain Imaging**

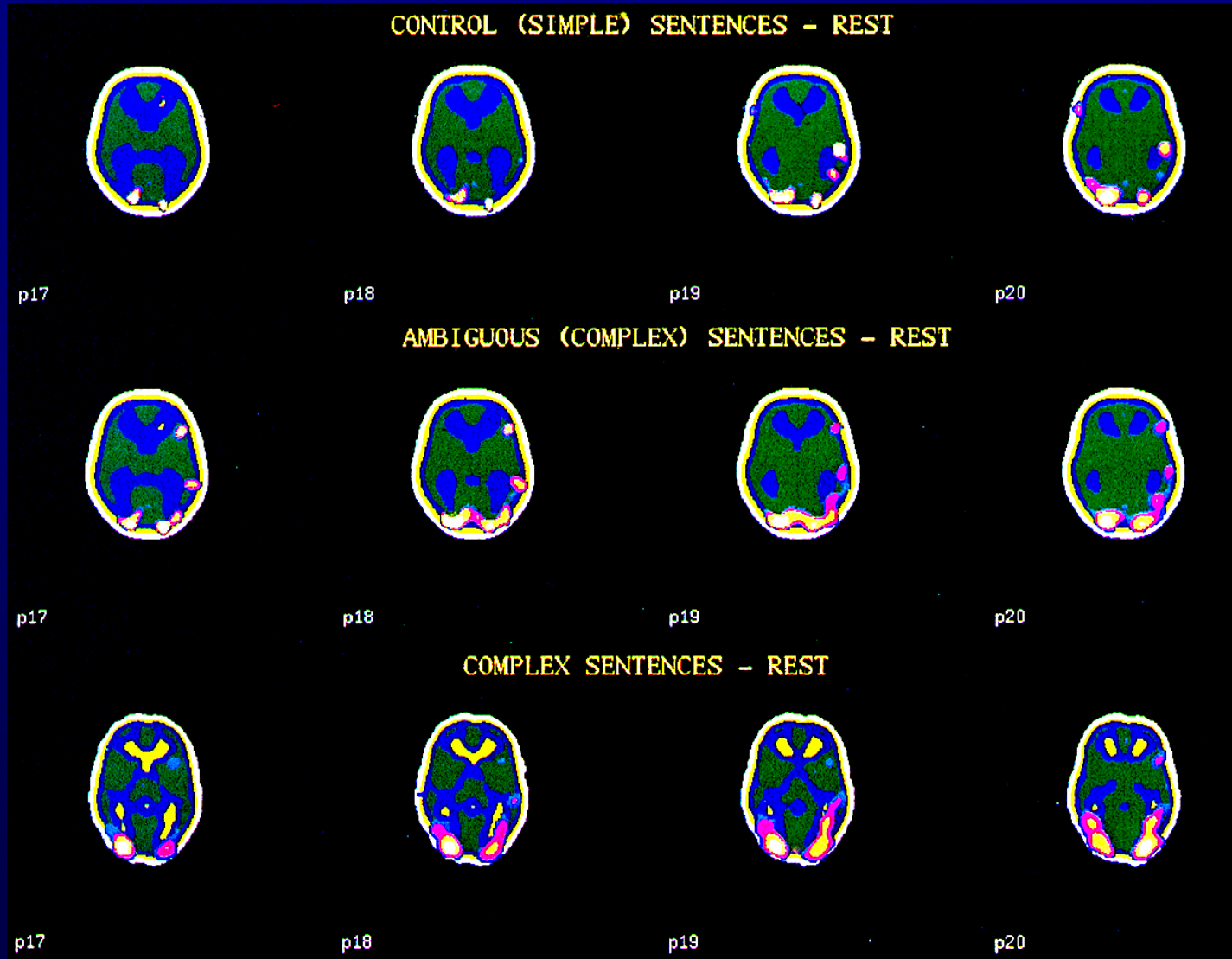
### **Complex Dutch Sentence**

**Of hogere straffen waartegen rechters protesteren dergelijke ongevallen voorkomen kan betwijfeld worden.**

### **Ambiguous Dutch Sentence**

**Zij kunnen bakken met zulk deeg niet verplaatsen.**







# Language localization in case of LTL arachnoid cyst

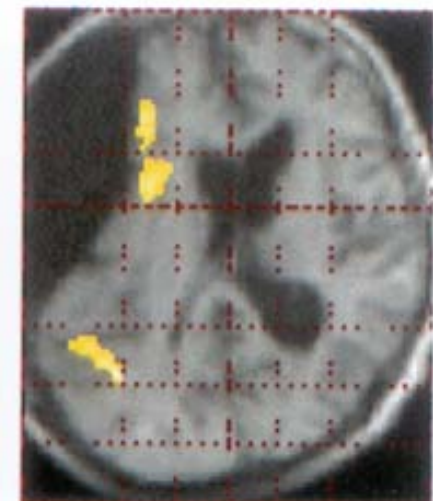
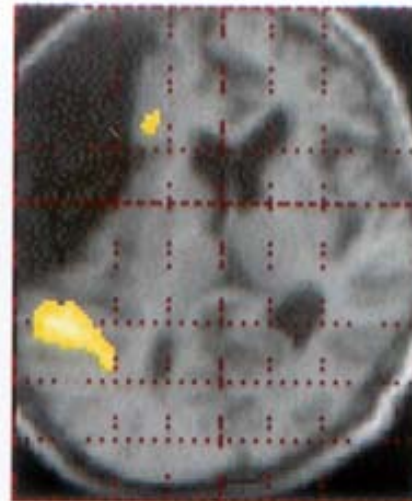
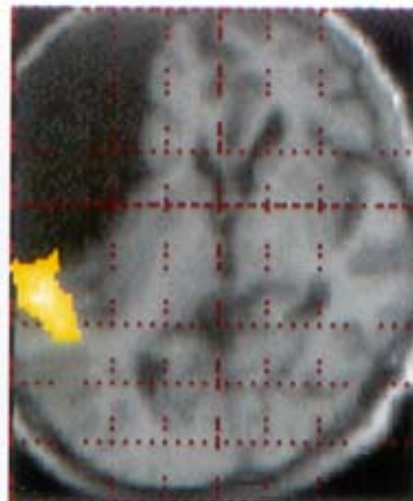
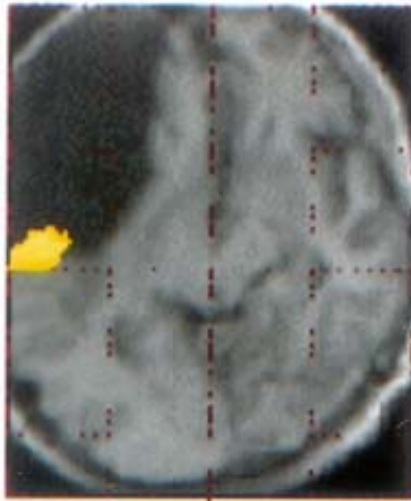
Case 2: Cutoff  $Z p = .001$

$z = -8\text{mm}$

$z = 0\text{mm}$

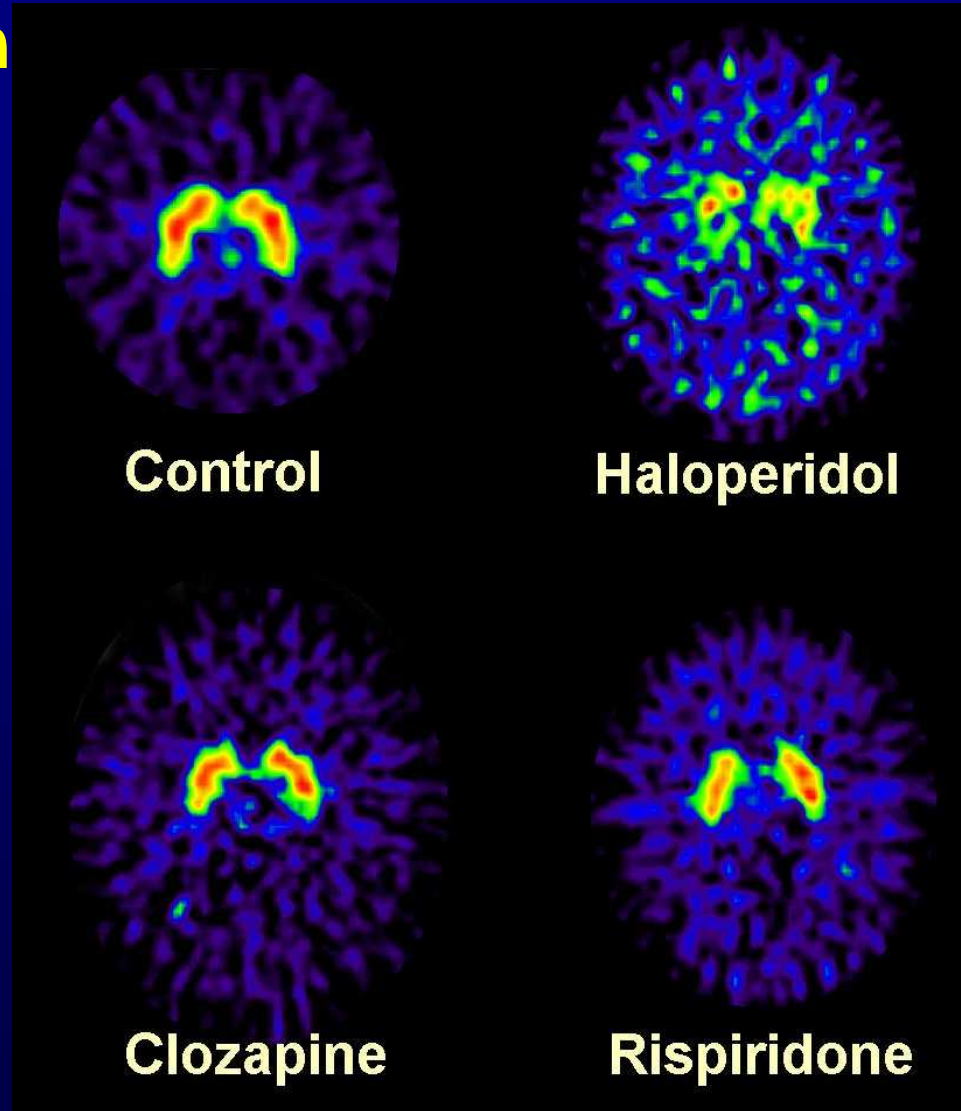
$z = 8\text{mm}$

$z = 16\text{mm}$





# FESP and medication





## Cardiac research

- Flow

$^{13}\text{NH}_3$ ,  $\text{H}_2^{15}\text{O}$ ,  $^{82}\text{Rb}$

- Metabolism  
acetate

$^{18}\text{FDG}$ ,  $^{11}\text{C}$ -fatty acids,  $^{11}\text{C}$ -

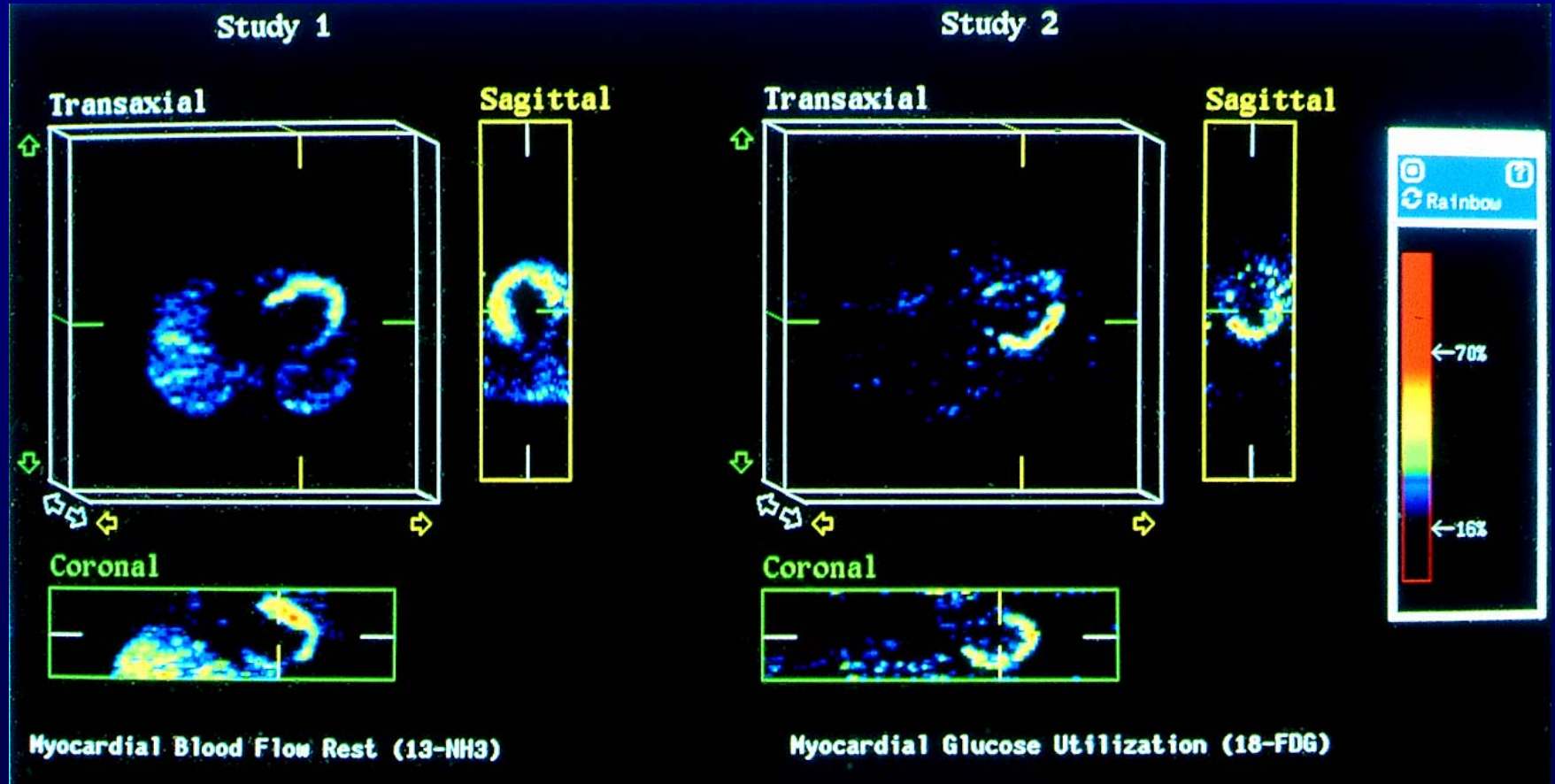
- Hypoxia

$^{18}\text{F}$ -fluoromisonidazole

- Receptors

$^{11}\text{C}$ -CGP-12177





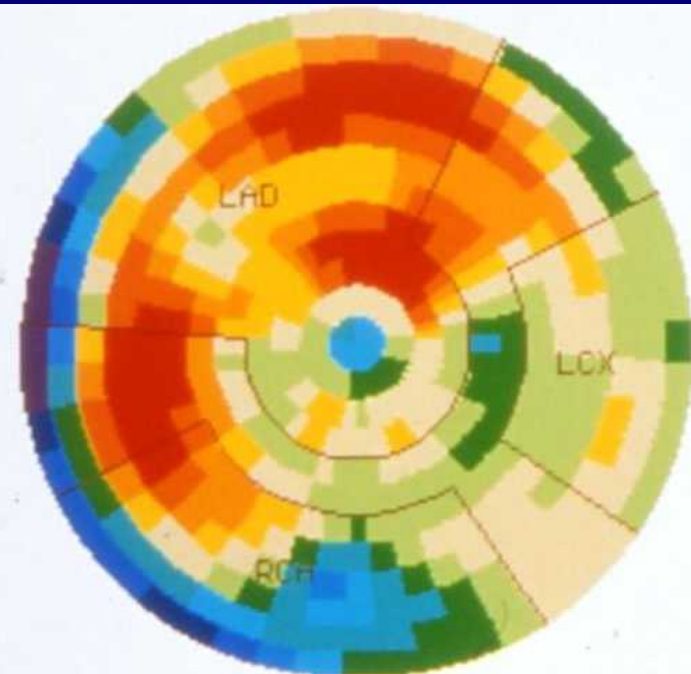
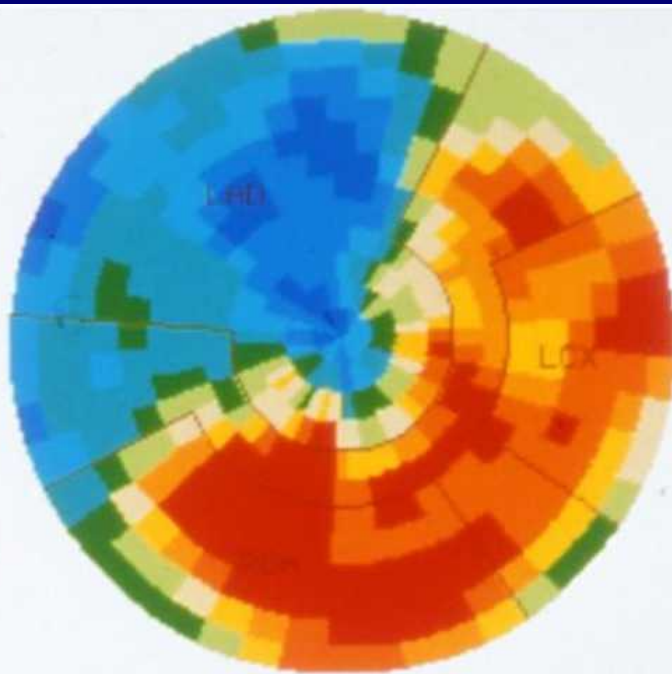
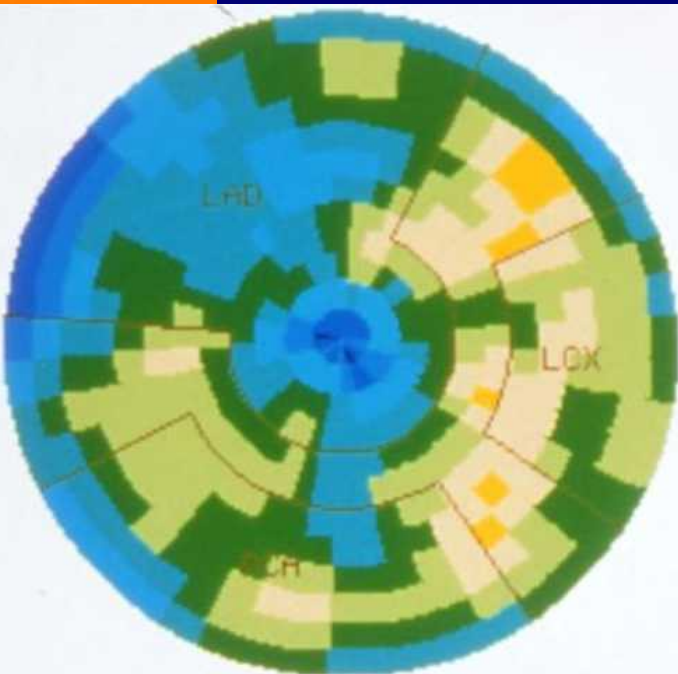


# Bypass surgery: yes or no?

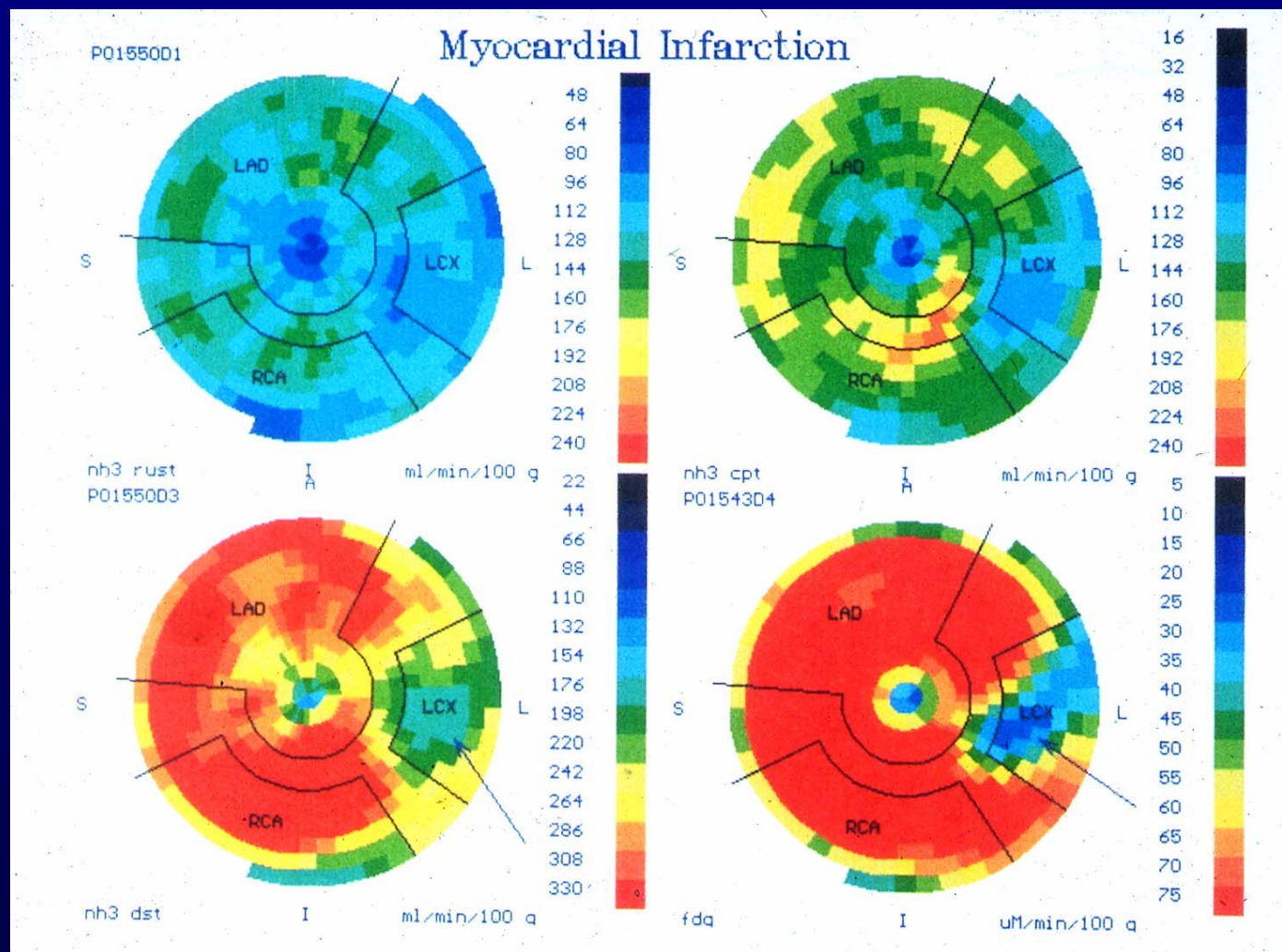
Flow at rest

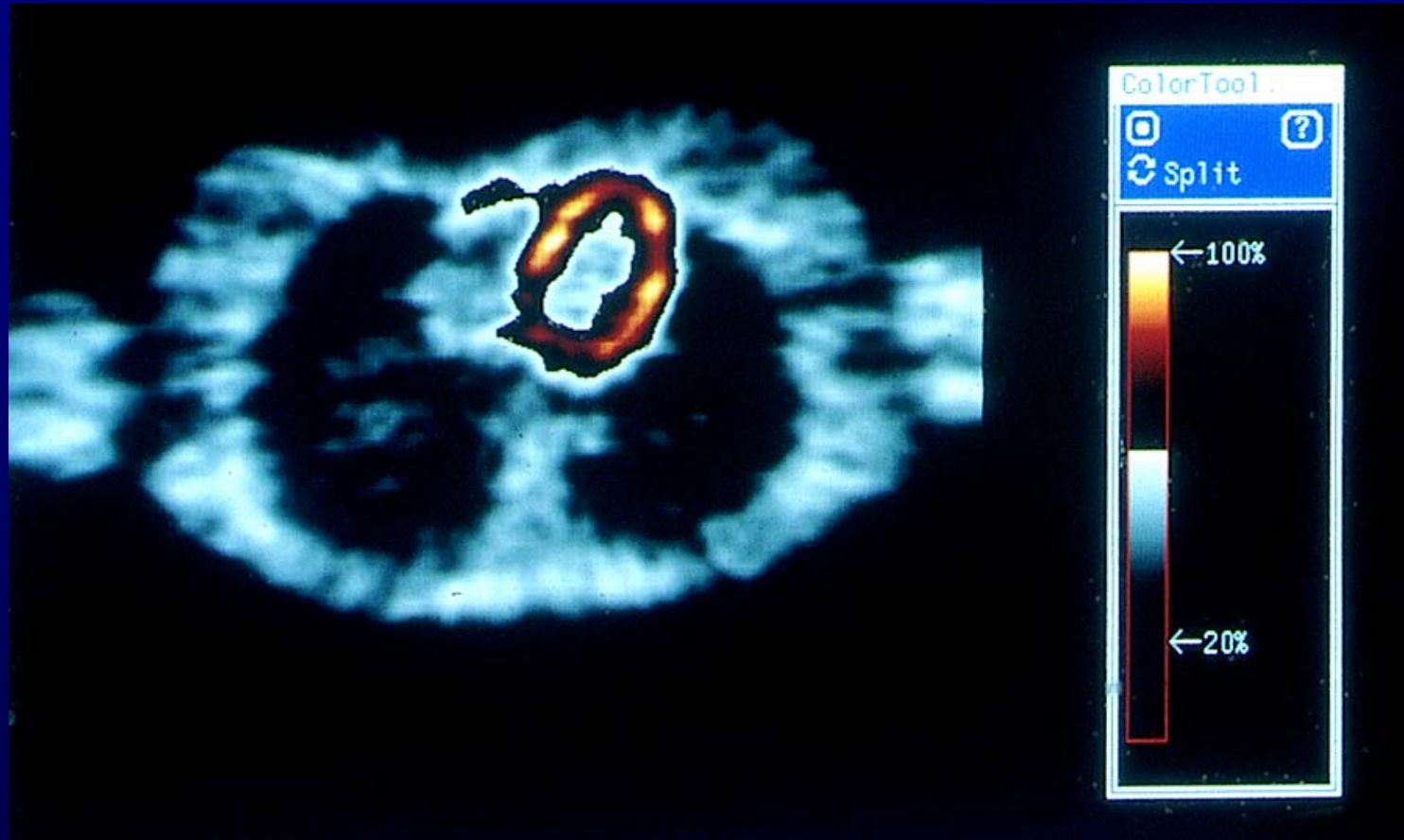
Flow at stress

Glucoseconsumption











## Oncological research

- Tumor flow

$^{13}\text{NH}_3$ ,  $\text{H}_2^{15}\text{O}$

- Tumor metabolism

$^{18}\text{FDG}$ ,  $^{11}\text{C}$ -tyrosine,  $^{11}\text{C}$ -methionine,  
 $^{11}\text{C}$ -thymidine,  $^{18}\text{FLT}$

- Cytostatic kinetics

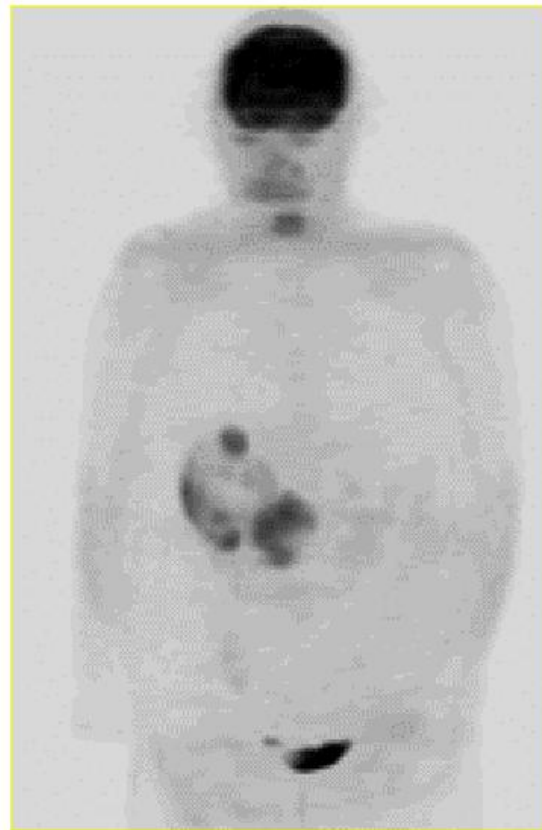
$^{11}\text{C}$ -cytostatics

- Therapy monitoring

Change in metabolism



# Therapy evaluation



VOOR

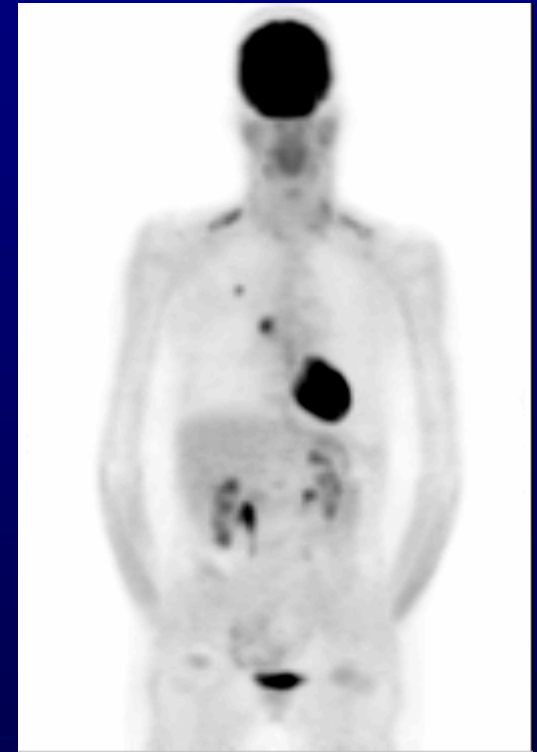


1 WEEK NA BEHANDELING



# Data Analysis of PET Data

- **Visual analysis**
- **Normalised uptake (SUV)**
- **Pharmacokinetic modelling**







# PET/CT

## the Siemens solution

# NM

Diagnostic  
Imaging Workshop

Siemens medical  
Solutions that help

SIEMENS

4

### Biograph: The imager for life



- ECAT EXACT HR+: High performance PET scanner
- ECAT Accel: High throughput PET scanner
- Siemens Somatom Emotion: High performance, spiral CT
- 70 cm patient port
- Optimized bed design
- Siemens syngo-based computer system





# Attenuation correction

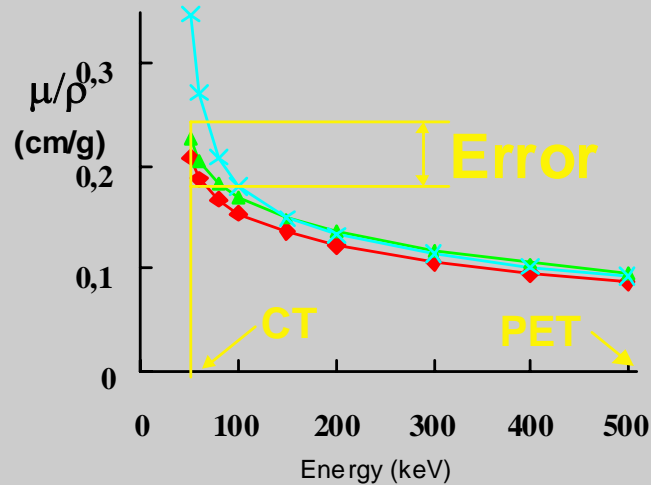
at CT energy (~ 70 keV)

at PET energy (511 keV)

# NM

## SIEMENS

### CT Attenuation Correction



- Hybrid method:
- segment bone in CT
  - scale bone by 0.44
  - scale other by 0.54

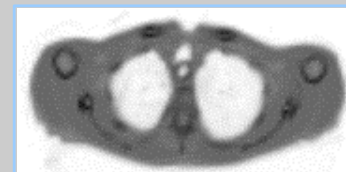
Photoelectric effect is higher in bone

Diagnostic Imaging Workshop

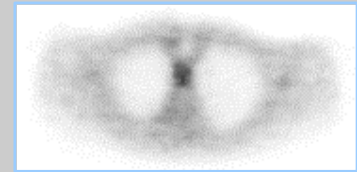
Siemens medical Solutions that help



Original CT scan



Scaled CT scan



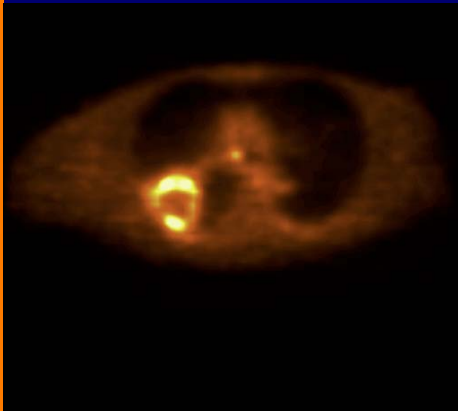
PET emission scan

Courtesy of the University of Pittsburgh Medical Center



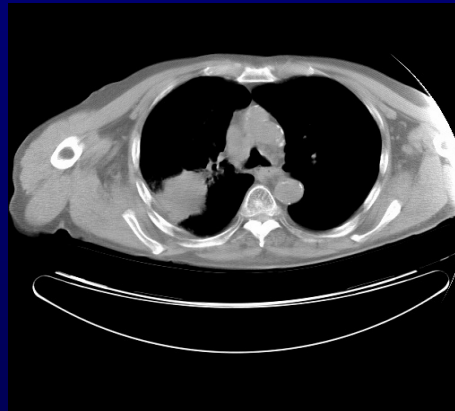
# Camera development: PET/CT

- **Hardware fusion**



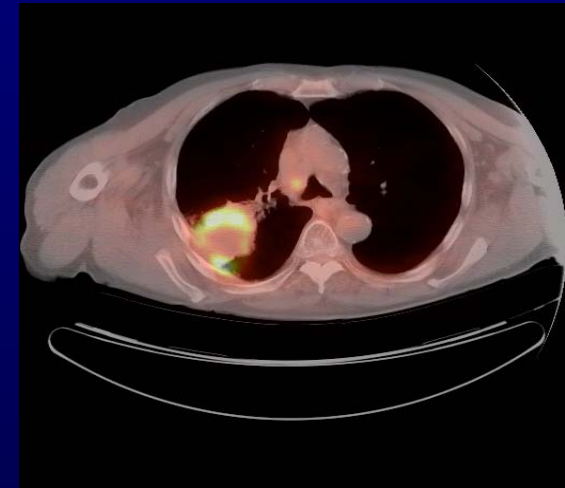
PET

+

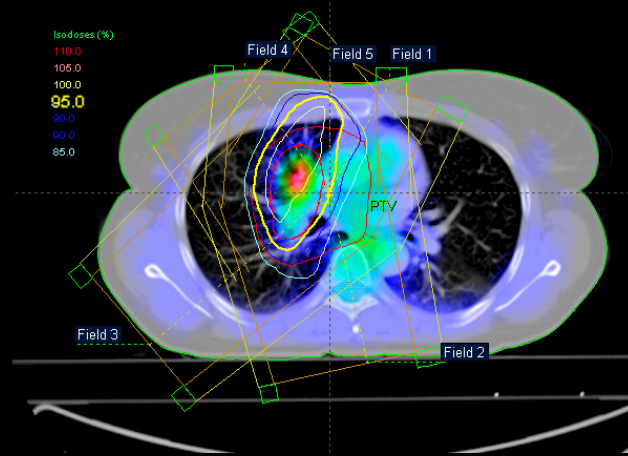
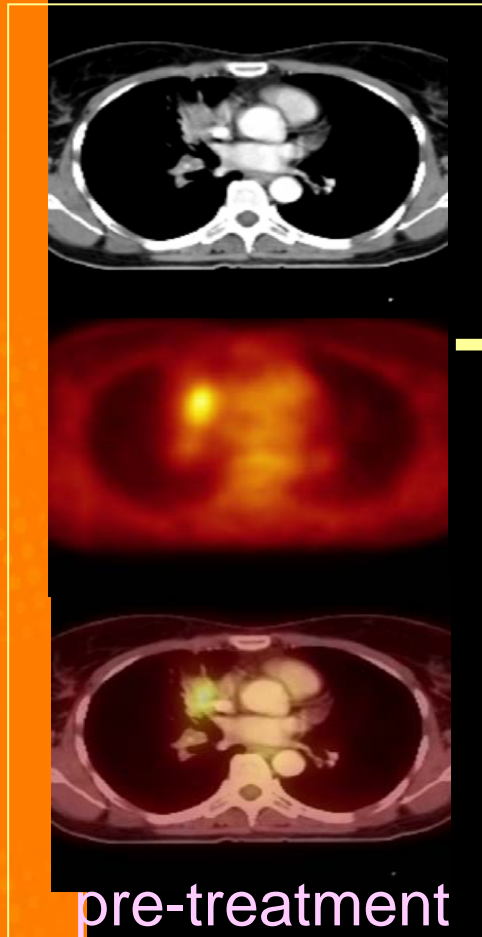


CT

=



PET/CT



## Treatment plan

### RT planning and response

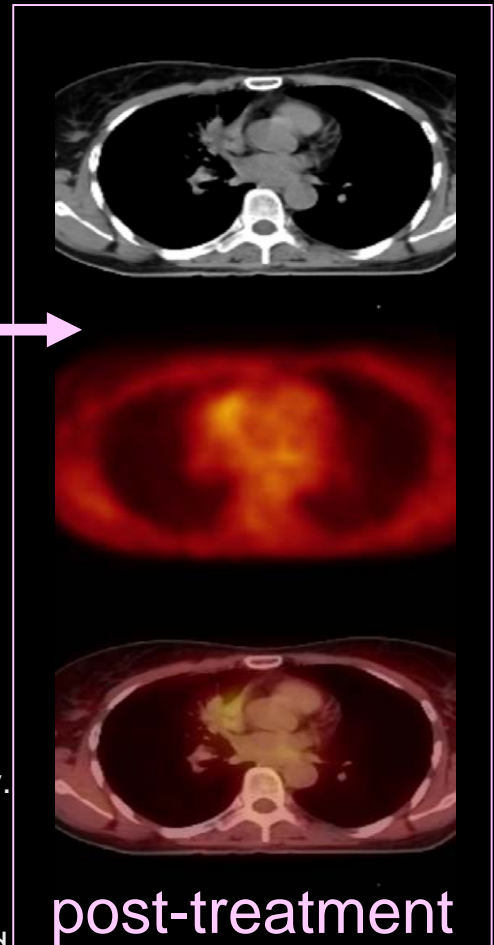
Case: Female with bronchial CA for RTP.

**Scan protocol:**

Standard whole-body PET/CT scan pre- and post-therapy. Pre- and post-therapy PET/CT can be registered using manual syngo-fusion tool.

**Findings:**

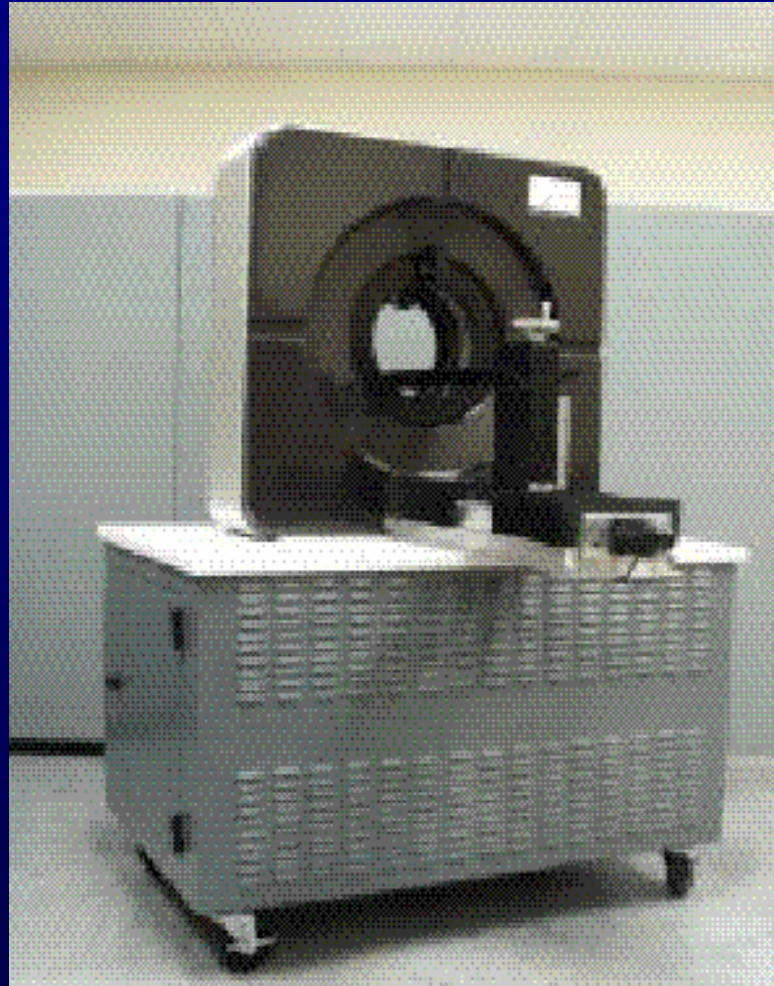
Evaluate extent of disease prior to RT. RT planning based CT or PET/CT. Evaluate RT response.



Data Courtesy of University Essen (Dr s S Marnitz and S Mueller)

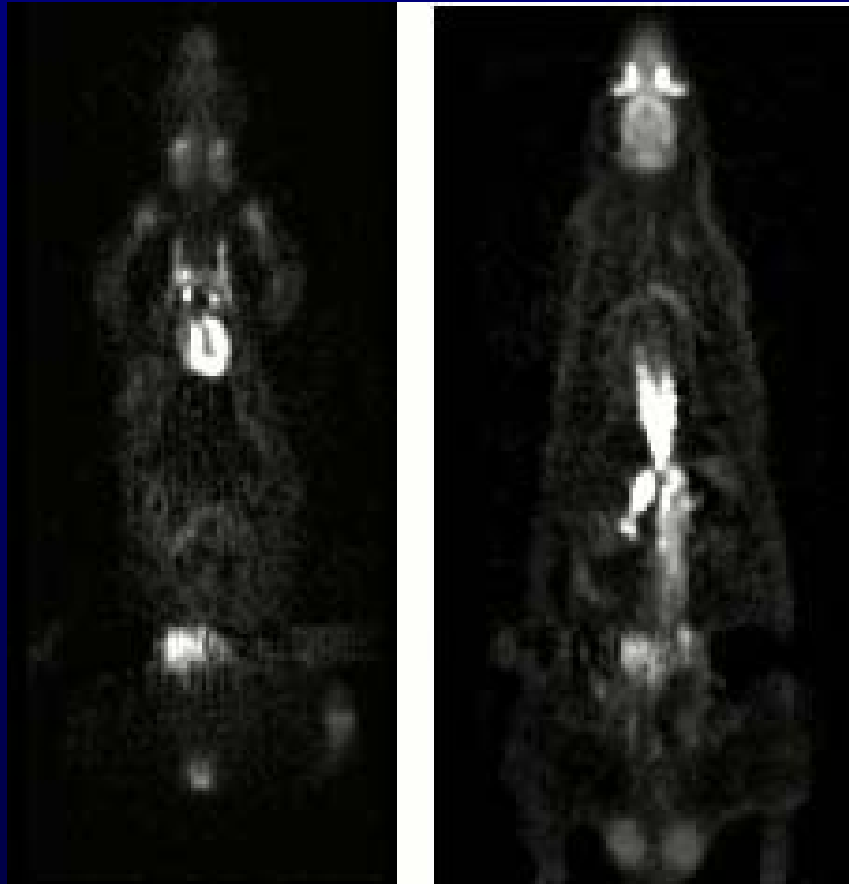


# MicroPET-P4





## $^{18}\text{F}$ FDG-Whole body rat images with MicroPET





# $^{11}\text{C}$ -WIN 35,428 for Pre-synaptic DA-transport imaging

**Monkey**

**Rat**

**Mouse**

